Noninvasive measurement of three-dimensional morphology of adhered animal cells employing phase-shifting laser microscope

Mutsumi Takagi
Takayuki Kitabayashi
Syunsuke Ito
Masashi Fujivara
Hokkaido University
Graduate School of Engineering
Division of Biotechnology and Macromolecular Chemistry
Sapporo 060-8628, Japan
E-mail: takagi-m@eng.hokudai.ac.jp

Akio Tokuda
FK Optical Laboratory
1-13-4 Nakano, Ni-iza
Saitama 352-0005, Japan

1 Introduction

Animal cell cultivation is a very important technology for pharmaceutical production and cell processing for regenerative medicine. To optimize and control the quality of cells during cultivation, monitoring of cell quantity and quality can be carried out nondestructively and noninvasively, especially in cell processing for transplantation and regenerative medicine. Although light microscopic observation is useful for the noninvasive monitoring of adhered animal cells, this technique cannot facilitate 3-D morphological observation, but only 2-D morphological observation.

An atomic force microscope (AFM) can be used to observe the 3-D morphology of adhered animal cells. For example, the differences in 3-D morphology between Chinese hamster ovary (CHO) cells cultivated under various osmolarities were measured under AFM after fixation treatment of cells.\(^\text{1}\) Because 3-D observation of adhered animal cells using AFM requires a long time and fixing treatment of cells, AFM observation is considered invasive for cells.

Recently, a novel phase-shifting laser microscope (PLM) was developed.\(^\text{2}\) A biprism, located between the magnifying lens and the observation plane, was used as a beamsplitter. (Fig. 1) The biprism was laterally translated to introduce phase shifts required for quantitative phase measurement with a phase-shifting technique. Namely, the phase shift (\(\Delta \Phi\)) caused by the difference in refractive indices between the sample and the reference expressed in Eq. (1) can be determined using PLM.

\[
\Delta \Phi = 2 \pi d \frac{n_1 - n_0}{\lambda_0},
\]

where \(\Delta \Phi\) is the phase shift (\(\cdot\)); \(d\) is the thickness of the sample (nanometers); \(\lambda_0\) is the wavelength of the laser (nm); and \(n_1\) and \(n_0\) are the refractive indices of the sample and reference (\(\cdot\)), respectively. We believe that PLM may be applicable for measuring the thickness (\(d\)) of living adhered cells by substituting the refractive indices of cells and the medium to \(n_1\) and \(n_0\) in Eq. (1), respectively.

In this study, noninvasive 3-D observation of animal cells under PLM without fixing treatment was investigated.

Abstract. Noninvasive measurement of 3-D morphology of adhered animal cells employing a phase-shifting laser microscope (PLM) is investigated, in which the phase shift for each pixel in the view field caused by cell height and the difference in refractive indices between the cells and the medium is determined. By employing saline with different refractive indices instead of a culture medium, the refractive index of the cells, which is necessary for the determination of cell height, is determined under PLM. The observed height of Chinese hamster ovary (CHO) cells cultivated under higher osmolarity is lower than that of the cells cultivated under physiological osmolarity, which is in agreement with previous data observed under an atomic force microscope (AFM). Maximum heights of human bone marrow mesenchymal stem cells and human umbilical cord vein endothelial cells measured under PLM and AFM agree well with each other. The maximum height of nonadherent spherical CHO cells observed under PLM is comparable to the cell diameter measured under a phase contrast inverted microscope. Laser irradiation, which is necessary for the observation under PLM, did not affect 3-D cell morphology. In conclusion, 3-D morphology of adhered animal cells can be noninvasively measured under PLM. © 2007 Society of Photo-Optical Instrumentation Engineers. [DOI: 10.1117/1.2779350]

Keywords: morphology; noninvasive; three dimensional; laser microscope.

Paper 06215R received Aug. 8, 2006; revised manuscript received Mar. 19, 2007; accepted for publication May 15, 2007; published online Sep. 12, 2007.
2 Materials and Methods

2.1 Cells and Media

Tissue plasminogen activator (tPA)-producing Chinese hamster ovary (CHO) 1-15500 cells (ATCC CRL-9606) were used. Ham’s F-12K medium (Dainippon Seiyaku Company, Limited, Japan) supplemented with 10% newborn bovine serum (NBS, Gibco, New York), streptomycin (0.1 mg/L), and penicillin (100 u/L) was employed for cell growth. Medium osmolarity was adjusted to 300 and 400 mOsm/L by the addition of NaCl solution (100 g/L). Medium osmolarity was determined by measuring the depression of the freezing point using an osmometer (model OM-801, Vogel, Germany). CHO cells (6.7×10^4 cells) were inoculated into 2 ml of the medium in a dish (Falcon, 9.6 cm²) and incubated for 4 days in a CO₂ incubator (37°C, 5% CO₂). Cell suspension was prepared by trypsinization of adhered cells on a dish.

Human bone marrow mesenchymal stem cells (MSCs) were isolated from bone marrow aspirate obtained by routine iliac crest aspiration from human donors (age 65 to 73) as previously reported. The content of CD105⁺ CD45⁻ cells among the cells analyzed by a flowcytometer was approximately 90% (data not shown). MSCs were cultured at densities of 0.15×10⁴ cells/cm² employing DMEM-LG (Gibco, New York) supplemented with 10% Fetal Calf Serum (FCS) (Gibco), 2500 U/L penicillin, and 2.5 mg/l streptomycin. Human umbilical cord vein endothelial cells (HUVEC) were purchased from Cambrex Bio Science Walkersville, Incorporated (Maryland) and cultured at densities of 0.2×10⁴ cells/cm² employing DMEM (Gibco, Japan) supplemented with 10% inactivated fetal bovine serum (Gibco), 1 aliquot (of the same concentration as that in MEM) of MEM nonessential amino acids (Gibco), 2-mM glutamine, 5000 U/L penicillin, and 5 mg/L streptomycin (Sigma, Missouri).

2.2 Cell Morphology Analysis under Phase-Shifting Laser Microscope

The adhered cells on the bottom surface of the culture dish were observed under PLM. Two neighboring fields of view with cells and without cells were selected as sample and reference fields, respectively, and phase shift (ΔΦ) was determined for all pixels in the sample field under PLM. By substituting the wavelength of the laser (λₒ=632.8 nm), the refractive indices of the cells determined by the method mentioned later (n₁=1.39, 1.375, and 1.375 for CHO, MSC, and HUVEC, respectively) and the medium (nₒ=1.34), and the measured phase shift (ΔΦ) to Eq. (2), the height of the cells (d nm) was calculated for all pixels in the sample field, and a 3-D view of the sample field was made.

\[ d = \frac{\Delta \Phi}{2 \pi} \times \frac{\lambda_o}{n_1 - n_0} \]  \hspace{1cm} (2)

2.3 Determination of Refractive Index of Cells

The culture medium was replaced with saline containing different concentrations of bovine serum albumin (380 to 480 g/L), in which osmolarity was adjusted to the original medium osmolarity, and cells were observed under PLM. The refractive index of the saline, with which cell images disappeared under PLM, was considered as the refractive index of the cells. The refractive indices of the medium and saline were determined using a refractometer (DR-A1, Atago Company, Tokyo, Japan).

2.4 Cell Observation under Atomic Force Microscope

Cells were fixed with glutaraldehyde (4%), dried, and analyzed using an atomic force microscope (AFM) (NanoScope...
IIIa, Veeco. Namely, the height was scanned for all parts of each cell, and the closed area showing positive height was defined as the cell adhesive area.5

3 Results and Discussion

3.1 Determination of Refractive Index of Adhered Chinese Hamster Ovary Cells

After the CHO cells in the culture medium were observed under PLM, the culture medium was replaced with saline containing albumin while the culture dish was fixed on the stage of PLM. Cell image was distinct with the saline, having refractive indices of 1.33 and 1.34 (Fig. 2). Cell image was indistinct for the saline refractive index of 1.38 and was not observed for the saline refractive index of 1.39. Consequently, the refractive index of the observed CHO cells was determined to be 1.39.

The refractive index of the cell membrane (1.5) is higher than that of the cytoplasm (1.35),6 and the thickness of the cell membrane is approximately 7.5 nm.7 Because the adopted refractive index for CHO cells in this study (1.39) was between 1.35 and 1.5, it may be the sum of the refractive indices of the cell membrane and cytoplasm. However, the digit of significant figures must increase to increase the accuracy of the cell height measurement under PLM in the future, because the difference in refractive index between the cells and the medium was small (e.g., 0.05).

3.2 Effect of Osmolarity on Three-Dimensional Cell Morphology Observed under Phase-Shifting Laser Microscope

CHO cells cultivated for 4 d under different osmolarities of 300 and 400 mOsm/L were observed under PLM [Figs. 3(a) and 3(b)]. The 2-D morphology of the CHO cells cultivated under 400 mOsm/L was elongated, while that of the CHO cells cultivated under 300 mOsm/L was globular. This difference in the 2-D cell morphology between the CHO cells cultivated under different osmolarities is in agreement with previous observations not only under AFM, but also under a conventional light-inverted microscope.1

The height of the CHO cells cultivated under 400 mOsm/L [Fig. 3(b)] was lower than that of the CHO cells cultivated under 300 mOsm/L [Fig. 3(a)]. The comparison of the average value for each ten cells showed that the cell maximum height under 400 mOsm/L was apparently lower than that under 300 mOsm/L (Fig. 4). This dependency of cell height on osmolarity is in agreement with a previous report observed under AFM.1 Moreover, there was no marked difference between the measured values under PLM and AFM.
Table 1 Cell maximum height measurement under PLM and AFM. The maximum height of each cell (n=10, mean±SD) observed under PLM and AFM are shown.

<table>
<thead>
<tr>
<th>Cell species</th>
<th>Cell maximum height (μm)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>PLM</td>
</tr>
<tr>
<td>CHO</td>
<td>2.00±0.92</td>
</tr>
<tr>
<td>MSC</td>
<td>1.52±0.79</td>
</tr>
<tr>
<td>HUVEC</td>
<td>1.09±0.92</td>
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These results strongly suggest the accuracy of cell height measurement using PLM.

3.3 Comparison of Maximum Cell Heights Measured by Phase-Shifting Laser Microscope and Atomic Force Microscope for Various Cell Species

To confirm the accuracy of measured cell height under PLM and the applicability of PLM to various kinds of animal cells, adhesive CHO, MSC, and HUVEC cells were observed under PLM without fixation and AFM with fixation and drying (Table 1). Average cell height of CHO cells was higher than those of MSC and HUVEC in both measurements of PLM and AFM. Average cell height of MSC cells were between those of CHO and HUVEC in both measurements of PLM and AFM. Average cell heights measured by PLM were near to those measured by AFM in all cell kinds, while the standard deviations for PLM measurement were a little larger than those for AFM measurement. These data can show that the accuracy of cell height measurement by PLM and PLM measurement should be applicable to various cell species.

Table 2 Observation of nonadherent CHO cells under PLM. Diameter and maximum height of nonadherent spherical CHO cells were measured by the observation under PLM and inverted phase contrast microscope. Mean±SD (n=10) are shown.

<table>
<thead>
<tr>
<th>Cell maximum height (μm)</th>
<th>Cell diameter (μm)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>PLM</td>
</tr>
<tr>
<td>5.68±2.53</td>
<td>7.33±1.49</td>
</tr>
</tbody>
</table>

maximum height (5.68±2.53) measured by PLM was smaller than the horizontal diameter (7.33±1.49) measured by PLM. This shows that cell height was a little smaller than the horizontal diameter due to the gravity force. These data support the accuracy of cell height measurement by PLM.

3.5 Influence of Laser Irradiation on Cell Morphology

To confirm the influence of laser irradiation required for PLM observation on cell morphology, a dish containing adhered CHO cells was set on the stage of a PLM and received continuous irradiation of a laser for 10 min, during which a 3-D cell morphology was observed at 0, 5, and 10 min, respectively (Fig. 5). There was no marked change in the 3-D cell morphology of the CHO cells during the laser irradiation for 10 min.

The laser irradiation dose required for PLM observation was less than 0.1 mW, and may not influence 3-D cell morphology, because an observation of one sample under PLM took only 30 s.

The spatial resolution in cell height observed under PLM should be approximately 10 to 2 nm, because the resolution in phase shift is 10 to 5 rad and the difference in refractive index between cell and medium is 0.04. This resolution under PLM might be comparable with or better than that observed under AFM. Cells adhered on the bottom of a conventional culture dish can be observed under PLM in situ together with culture medium, while cells need to attach onto some special board and liquid culture medium should be removed for observation under AFM. So, PLM observation might be noninvasive compared to AFM observation. Observation of cells under PLM takes only a few minutes and needs no special training, because 3-D morphology can be observed for voluntary cells selected under a normal light inverted microscope. Moreover,
there is almost no restriction for cell height observed under PLM, while cell height observed under AFM is limited by the size of the lever (e.g., 5 μm). Consequently, the observation of 3-D cell morphology under PLM might be more attractive for academic and pharmaceutical research compared to AFM observation.

4 Conclusion
These data show that PLM can quantitatively measure the 3-D morphology of adhesive animal cells noninvasively.

References