Optical coherence tomography in gynecology: a narrative review

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1 Introduction

Modern clinical practice demonstrates a strong requirement for noninvasive diagnostics techniques capable of providing improved diagnostic efficiency. Among other medical areas, this demand is especially sounding in gynecology, where the problems of untimely diagnostics of neoplasia and latent inflammations affect female reproductive function or lead to cancer development.

While the incidence of invasive cervical cancer has decreased in the last three decades, the rate of cervical dysplasia has significantly increased, especially in women of reproductive age. In this respect, diagnosis, management, and follow-up of preinvasive cervical lesions are now a major public health challenge. Combination of colposcopy and directed biopsy is currently an accepted management technique; however, it has low specificity resulting in a fairly large absolute number of overtreatment cases. Previous studies have shown that unnecessary invasive diagnostic procedures often lead to associated complications, including adverse birth outcomes.

In diagnostics of inflammatory diseases and reproductive disorders, laparoscopy is a standard procedure for examining pelvic pathologies; however, the origin of disorders often cannot be revealed. Disorders in female fertility are often caused by chronic inflammatory processes within the uterus. Hysteroscopy, a standard diagnostic tool based on macroscopic examination, reveals chronic endometritis in only 35% of cases and should be complemented by an invasive endometrial biopsy. In this respect, noninvasive diagnostic techniques for gynecology applications are required.

Optical coherence tomography (OCT) is a modern imaging modality capable of providing images of biotissue structure with micron-range spatial resolution anticipated in the late 1980s. Recent achievements in OCT technology provide imaging of biotissues with resolution down to units of microns at depths up to units of mm. After pioneering applications in ophthalmology, OCT was actively introduced into other clinical areas, including gynecology. Pioneering clinical applications of OCT in gynecology go back to the late 1990s when the first in vivo OCT images of cervix in norm and in course of neoplasia development were obtained. OCT images of pelvic organs (ovaries and fallopian tubes) were obtained in course of standard laparoscopy procedure, and OCT images of endometrium were obtained in course of hysteroscopy. Furthermore, the OCT studies in gynecology were directed toward revealing the capabilities of OCT in monitoring pathomorphologic and pathophysiologic alterations, which can be used both for diagnostics and treatment monitoring. The first ex vivo study in gynecologic OCT demonstrated the capability of human oviduct imaging of samples after hysterectomy for leiomyomatosis. An in vitro study demonstrated that, in OCT images of cervical and uterine tissues in norm and pathology stressing, OCT provides imaging at a resolution higher than any currently available noninvasive clinical imaging technology. Another study on postmortem samples of endometrium and ovary compared OCT images with histology and demonstrated capabilities of OCT in diagnostics of endometritis and ovary neoplasms, and the high potential of laparoscopic OCT applications was emphasized.

Further progress in the introduction of OCT into clinical gynecologic practice aimed at developing customized OCT probes suitable for standard diagnostic procedures and accumulation of OCT image atlases of pelvic organ tissues in norm and pathologies. Recent studies concentrated on application of OCT for nontumor gynecologic pathologies while development of numerical processing and diagnostic image quantification increased diagnostic accuracy against both sole application of standard diagnostic techniques and visual evaluation of diagnostic OCT images.
The structure of this review is organized as follows: Sec. 2 reviews the technical customization aimed at making OCT technology most compatible with standard diagnostic gynecologic procedures and the combination of OCT with other modern diagnostic modalities. Section 3 overviews the application of OCT for revealing and classification of neoplasia of gynecologic localization, while Sec. 4 discusses the application of OCT for detection of inflammatory diseases and treatment monitoring, paying special attention to application of numerical methods for diagnostic accuracy enhancement. The essential inclusion criterion for this review was reporting either ex vivo or in vivo results on OCT inspection of human female reproductive organs tissue starting from the late 1990s until now.

2 Customization of Optical Coherence Tomography Probes for Gynecology Applications

One of the essential aims of OCT customization for gynecologic applications is the construction of the fiber-optic-based system equipped with the probe compatible with standard hysteroscopes. While inspection of cervix and vulva does not require special probe configuration and standard laparoscopes employed for fallopian tubes inspection are compatible with most fiber-optic probes, inspection of uterus requires customization, and compatibility of an OCT probe with a hysteroscope is challenging. The first trials on OCT hysteroscopy were performed with a system with a fiber-optics probe with a diameter of 2.7 mm, compatible with a rigid hysteroscope. The further development of this technology, its enhancement by employing polarization-sensitive OCT imaging, and clinical applications are overviewed in Ref. 20.

In addition to miniaturization, a way to enhance OCT probes consists of the ability for circular and three-dimensional (3-D) scanning; although such systems are usually not compatible with hysteroscopes, they can be efficiently used for OCT colposcopy. A recent paper reports on an OCT system for colposcopy featuring two probe designs. The first design allows for circular scanning while the other is capable of 3-D imaging over a 4.6 × 4.6 mm² area.

A particular issue to be accounted for when using contact fiber-optics probes is tissue compression induced by contact of the probe with tissue surface. The probe pressure to the tissue may induce deformation, affecting the optical properties of tissue and, thus, the OCT image. A special device conjugated with fiber-optics OCT probe was reported in Ref. 22, allowing control of probe pressure in course of OCT colposcopy.

Another approach stimulating development of OCT probes for gynecologic applications is the combination of OCT with other diagnostic modalities, including both standard and perspectives. Complementary use of OCT imaging and positron detection resulted in the development of a fiber-based probe where the Fourier-domain OCT for volumetric imaging is surrounded by plastic scintillating fiber tips for preferential detection of local positron activity. The system is aimed at intraoperative detection of ovary cancer.

Another combination method proposed for diagnostics of ovarian cancer includes OCT, ultrasound (US), and photoacoustic imaging (PAI). The overall diameter of the modularity probe of the developed system is 5 mm, which is suitable for a standard 5- to 12.5-mm endoscopic/laparoscopic port. The probe combines a ball-lensed OCT sample arm probe, a multimode fiber for PAI, and a high-frequency US transducer with 35-MHz center frequency. Simultaneous employment of PAI allows for blood vessel detection, especially at depths beyond the OCT imaging range.

Modern trends in optical biopsy tend to combine OCT with microscopy imaging. A recent study reports on the development of a combined OCT-microscopy system aimed at the detection of uterine cervix cancer. The system provides OCT imaging under microscopic guidance and was tested in ex vivo samples obtained by an electrosurgical excision procedure. The approach was demonstrated to be efficient in the detection of high-grade squamous intraepithelial lesions.

A recent study suggests that the fallopian tubes play an important role in the origin of ovarian cancer, making it a critical tissue to timely detect the pathology at an early stage. It was shown that fluorescence imaging of human ovarian and fallopian tube tissue is promising for early cancer detection. A combination of fluorescence-based techniques and OCT seems to provide additional benefits. An endoscopic probe for the conjugation of OCT with wide-field fallopyscopy, as well as multimodal imaging of ovarian tissue using OCT and second-harmonic generation microscopy, was also reported.

3 Optical Coherence Tomography Diagnostics of Cancer in Gynecology

3.1 Optical Coherence Tomography Diagnostics of Cervix

The growth of early forms of cervical neoplasia in women of reproductive age requires effective diagnosis. Traditional colposcopy suffers from low specificity that leads to an increasing number of invasive diagnostic procedures and overtreatment. Thus, there is a strong need for diagnostic techniques, preferably noninvasive, capable of detecting cervical neoplasia at early stages with high accuracy. OCT has extremely high potential as an efficient solution for this problem. The first clinical experience of OCT application for cervix diagnostic was gained in 1997 when typical OCT images of cervical tissue in norm and neoplasia were obtained. It was demonstrated that the OCT images of cervix in norm feature stratified squamous cell epithelium and connective tissue stroma with vessels, while a structureless image is an indicator of neoplasia. Typical images of cervix in norm and in cases of nontumor and tumor pathologies are shown in Fig. 1. In 1998 in Ref. 16, the differences in OCT images of cervix in patients with hypostrogenia and hyperestrogenia were demonstrated, manifested by the thickness and the density of the squamous epithelium. Separately, the images of cervix of unpregnant and pregnant women were compared. Typical images for patients with precancer state [cervical intraepithelial neoplasia (CIN) II] were also reported and qualitative criteria to distinguish precancer alterations were formulated. In a further study, 50 patients with CIN I, II, III, metaplasia/inflammation, and squamous cell carcinoma were enrolled. Typical images for all cases with higher spatial resolution as compared with a previous paper were obtained. It was demonstrated that OCT allows the separation of invasive cancer from a high-grade preinvasive form that potentially avoids unnecessary biopsies. Another group demonstrated the efficacy of OCT in distinguishing between normal and abnormal (human papillomavirus, CIN I to III) cervical tissue. Numerical scoring employing the average intensity of the OCT signal from the epithelial layer was developed, demonstrating higher accuracy in premenopausal patients as compared with postmenopausal.
As the next step, the sensitivity and specificity of OCT in the detection of cervical cancer in combination with traditional approaches, visual inspection with acetic acid (VIA) and colposcopy, were determined. Typical images of ectocervix for norm, chronic inflammation, carcinoma in situ, and CIN III were demonstrated. It was shown that OCT provides an increase in specificity in the detection of CIN II from 34% to 61% when used in combination with VIA as compared with VIA alone while sensitivity drops from 76% to 53%. Additional employment of colposcopy results in sensitivity of 46% and specificity of 69%. Similar evaluation of OCT efficacy alone in detecting cervical neoplasia was carried out later by another group reporting sensitivity values of 95% and 96% and specificity values of 46% and 29% for two independent investigators, while interobserver agreement kappa equal to 0.68 is reported. The continuation of this work reports high-resolution images of healthy cervical tissue, CIN I, II, and III together with corresponding histology images. Reported values for sensitivity are 98% and 96% for two investigators with specificity of 39% and 41%, respectively, when the threshold for tumor state is set at CIN I. Shifting the threshold to CIN II results in sensitivity of 86% and 84% while specificity dramatically rises to 64% and 60%, respectively. Similar to previous study, interobserver agreement kappa is reported as 0.69 and 0.62 for threshold of CIN I and CIN II, respectively.

The idea of combination of OCT inspection with VIA proposed in Ref. gains its continuation in another prospective study with 1000 patients enrolled. When the threshold was chosen as CIN II, the sensitivity and specificity of VIA only in detecting lesions were 43% and 96%, respectively, while in combination OCT the sensitivity increased to 62% with a specificity of 80%. The authors stress that introduction of the OCT-signal attenuation. Epidermis thickness was found as 6.2 mm in normal vulvar tissue and 2.1 mm for VIN, respectively. Furthermore, these criteria were extended to four classes of vulvar tissue represented by an epidermal layer with an underlying connective tissue layer, the approaches for employment OCT in evaluation of vulva pathologies are similar to that employed for cervix. In the pioneering paper in OCT inspection of vulva, the OCT images of vulva with Paget’s disease were reported and compared with corresponding histology images. In later studies, it was demonstrated that OCT is efficient in differentiating between normal and VIN tissue. Two criteria were employed for differentiation: the thickness of the epidermal layer measured from an OCT image and the attenuation coefficient of this layer extracted from in-depth OCT-signal attenuation. Epidermis thickness was found as 0.19 ± 0.04 mm in normal vulvar tissue and 0.56 ± 0.22 mm in VIN. The attenuation coefficient amounted to 2.1 ± 1.4 mm⁻¹ and 6.2 ± 2.1 mm⁻¹ for norm and VIN, respectively. Furthermore, these criteria were extended to four classes of OCT images of vulva: normal, benign, VIN, and vulvar squamous cell carcinoma (VSCC). It was demonstrated that use of epidermal thickness ensures distinguishing between normal/benign tissue and VIN/VSCC tissue with sensitivity of 100% and specificity of 80%. Employment of the attenuation coefficient provides sensitivity of 100% and specificity of 70%. OCT was demonstrated to be efficient in the detection of margins of VSCC, which is important for determining the stage of the disease.

### 3.2 Optical Coherence Tomography Diagnostics of Vulva

Recent years are characterized by the increase in vulvar intraepithelial neoplasia (VIN) occurrences requiring improved diagnostic techniques. Although cervical tissue is mucosa, while vulvar tissue is skin, due to similar morphologic structure of cervical tissue and vulvar tissue represented by an epidermal layer with an underlying connective tissue layer, the approaches for employment OCT in evaluation of vulva pathologies are similar to that employed for cervix. In the pioneering paper in OCT inspection of vulva, the OCT images of vulva with Paget’s disease were reported and compared with corresponding histology images. In later studies, it was demonstrated that OCT is efficient in differentiating between normal and VIN tissue. Two criteria were employed for differentiation: the thickness of the epidermal layer measured from an OCT image and the attenuation coefficient of this layer extracted from in-depth OCT-signal attenuation. Epidermis thickness was found as 0.19 ± 0.04 mm in normal vulvar tissue and 0.56 ± 0.22 mm in VIN. The attenuation coefficient amounted to 2.1 ± 1.4 mm⁻¹ and 6.2 ± 2.1 mm⁻¹ for norm and VIN, respectively. Furthermore, these criteria were extended to four classes of OCT images of vulva: normal, benign, VIN, and vulvar squamous cell carcinoma (VSCC). It was demonstrated that use of epidermal thickness ensures distinguishing between normal/benign tissue and VIN/VSCC tissue with sensitivity of 100% and specificity of 80%. Employment of the attenuation coefficient provides sensitivity of 100% and specificity of 70%. OCT was demonstrated to be efficient in the detection of margins of VSCC, which is important for determining the stage of the disease.
3.3 Optical Coherence Tomography Diagnostics of Ovary

Ovarian cancer ranks fifth in cancer deaths among women, accounting for more deaths than any other cancer of the female reproductive system. A woman’s risk of getting ovarian cancer during her lifetime is about 1 in 75, and a lifetime chance of dying from ovarian cancer is about 1 in 100. Survival is strongly associated with the stage of cancer at diagnosis; however, currently, there exist no efficient approaches for early detection and screening of ovarian cancer. One of potential approaches consists of complementary use of modern imaging techniques, including OCT.

For the first time, OCT images of ovarian tissue with cystadenocarcinoma and adenoma together with corresponding histology images were reported in 1999; the authors stressed a high potential of laparoscopic applications of OCT. A laparoscopic OCT device was employed for diagnostics of ovarian cancer in paper. The paper features OCT images of postmenopausal ovary in norm, endometriosis, serous cystadenoma, and endometrioid adenocarcinoma with corresponding histology images. Typical features of these OCT images were formulated.

A later study demonstrated the potential of combining OCT with PAI and US in vivo and positron detection ex vivo in revealing malignant areas in the ovary. In addition investigations the benefits from numerical processing of OCT images of ovary ex vivo were demonstrated for the obtained image set. The first study proposed employment of the use of scattering coefficient of the ovary tissue derived from an OCT image as a criterion to separate normal tissue from a malignant one. The coefficient is extracted basing on the confocal point spread function of the OCT system and Beer’s law. Reported values for normal and malignant groups are 2.41 ± 0.59 mm⁻¹ and 1.55 ± 0.46 mm⁻¹, respectively. The approach distinguished normal ovary from a malignant one with sensitivity from 80% to 61% and specificity from 75% to 90% when the threshold value varied from 2 to 1.67 mm⁻¹. The study analyzed angle-resolved scattering properties derived from OCT images when the scattering coefficient was derived for different directions of an A-scan, and the mean correlation coefficient for these values was calculated. It was shown that this coefficient is higher for normal tissue than for a malignant one, providing 100% specificity and sensitivity for the considered set of OCT images from 10 ex vivo ovaries. Additional benefits in detection malignancy in the ovary are provided by polarization-sensitive OCT modality providing both conventional OCT image and conjugated phase retardation map. Phase retardation map reflects the birefringence properties of the tissue, thus allowing evaluation of the collagen state. Disrupted collagen is usually an indicator of a malignancy presence. Average phase retardation value derived from phase retardation maps was employed as another criterion in line with scattering coefficient to separate norm from malignancy, providing sensitivity of 43% and specificity of 100%. Being used in combination with scattering coefficient, it ensured both specificity and sensitivity of 100%. An overview of employment of OCT for characterization of ovarian tissue was given in a review paper. Recent animal studies aimed at proving the efficacy of OCT in ovary transplantation demonstrated high potential of OCT in detecting metastases in the ovary, including micrometastases. A recent ex vivo study employing full-field OCT demonstrated that application of standard image characterization (calculation of mean, variance, skewness, kurtosis, and entropy) to OCT images of ovaries allowed to differentiate normal ovary from a malignant one with a sensitivity of 92% and specificity of 88%. It is worth mentioning that, despite quite extensive studies on OCT applications for detection of ovarian cancer, most of the works are ex vivo, and the technology is yet to be translated to clinical practice. The combination of OCT with a falloscope by a custom-designed probe tested in animal study is a significant step toward clinical application.

4 Optical Coherence Tomography Diagnostics of Nontumor Pathologies and Treatment Monitoring In Gynecology

Although the main role of OCT in gynecology as an in vivo technique of morphological inspection is the detection of cancer, it can serve as a tool for the detection and classification of other pathologies of gynecologic localizations, namely inflammatory diseases and their manifestation, such as edema, sclerosis, and others. The localizations include uterine cavity (endometrium pathologies), cervix, vulva, and fallopian tubes.

One of the pioneering papers on OCT in gynecology reported typical images of normal peritoneal surface of uterus and endometriosis with corresponding histology images. The ex vivo OCT images of normal peritoneal surface feature adipose tissue and underlying uterine myometrium while endometriosis was manifested by appearance of characteristic glandular structures. Later, OCT images of endometrioid foci were reported for in vivo studies.

Further laparoscopic OCT was used to diagnose fallopian tubes in cases of silent inflammation and infertility of unknown origin. OCT images of fallopian tubes with latent inflammation were obtained, and criteria for detection of chronic salpingitis with OCT were developed. A numerical approach for OCT image analysis aimed at scoring the feature of an OCT image typical for manifestations of sclerosis and edema was developed. Sclerosis is usually manifested by higher OCT-signal level associated with higher scattering while edema is manifested by well-shaped darker areas associated with presence of extracellular liquid. It was demonstrated that employment of OCT in addition to standard laparoscopy only increased sensitivity from 44% to 90% and specificity from 67% to 81%, while numerical scoring of OCT images achieved sensitivity and specificity of 100% and 96%, respectively, for a set of 61 OCT images. Typical images of fallopian tubes in norm and in cases of inflammation are shown in Fig. 2.

Recent studies report on the application of OCT for detection and classification of endometritis. Numerical processing of diagnostic OCT images allowed the development of a scoring system to quantify endometritis grade. The system is based on evaluation of the grade of sclerosis, which is a constant morphologic indicator of chronic endometritis. OCT studies of cervix also demonstrate that OCT can be a tool to evaluate the hormonal state of cervix reporting on differences in images for pre- and postmenopausal patients. The OCT technique also demonstrated to be efficient in revealing nontumor cervix alterations in combination with a mechanical compression approach when typical layered structure is not observed. Evaluation of a diagnostic OCT image of suspicious cervix region after inspection with controlled mechanical compression of an OCT probe to cervical tissue avoided unnecessary biopsies in particular cases.
OCT was also employed for evaluation of vaginal epithelial damage and monitoring of its treatment with nonoxynol-9 vaginal gel. Colposcopy was used simultaneously as a standard approach. Epithelial thickness and integrity were used as scores derived from OCT images to evaluate the state of the tissue. OCT revealed epithelial disruption and thinning not identified by colposcopy.

Animal studies demonstrated that high-resolution OCT can be used noninvasively to evaluate vaginal morphologic features, including epithelial thickness, to assess this protective barrier in transmission of sexually transmitted infections and to monitor tissue response to topical medications and hormonal fluctuations. In clinical studies, it was shown that cross-polarization OCT can be used for noninvasive monitoring of responses of tumors and adjacent normal tissues to photodynamic therapy (PDT) of cervical cancer, thus, being useful for evaluation of the effectiveness of therapy and for choosing optimal treatment tactics.

The potential of OCT in employment for screening programs in microbicenosis studies was also demonstrated.

5 Conclusion

Optical techniques are used for gynecologic applications due to their noninvasiveness and high diagnostic accuracy compared with traditional diagnostic techniques. OCT has a special potential in gynecologic applications due to high-resolution imaging, customized probes, and sensitivity to both morphologic and functional changes. The main advantages of applications of OCT technology in gynecology are noninvasiveness and ease of operation; generally, its usage is similar to that of US technology.

Employment of customized OCT probes, especially in combination with other diagnostic modalities, provides additional diagnostic information to avoid unnecessary biopsies. In diagnostics of tumor pathologies, OCT not only reveals the pathology to detect the stage of the disease and to plan the treatment. In particular cases, extremely high values for specificity and sensitivity are demonstrated with OCT while traditional techniques provide comparatively low diagnostic accuracy. Employment of OCT was demonstrated to be efficient in diagnostics of latent forms of inflammation, which is important in diagnostics of reproductive disorders in females.

The main drawbacks of the OCT employment in gynecology consist of high requirements of the OCT probes—in diagnostics of cervix and vulva, sterilization of the probes is critical; in diagnostics of ovaries and fallopian tubes, the probe geometry should fit a standard laparoscope; and in diagnostics of endometrium, it should fit a standard hysteroscope. Another OCT drawback is the requirement for correct interpretation of the obtained diagnostic OCT image, and a clinician who is not familiar with the technique may fail to provide a correct diagnosis. In this respect, numerical image processing and analysis are of importance, as they were demonstrated to increase the diagnostic accuracy of OCT in a number of gynecologic applications. An associated drawback, which follows from OCT studies of cervix being the most extensive investigation from all OCT gynecologic applications, is comparatively low specificity of OCT. Potential ways for increasing the specificity of OCT include application of image enhancement approaches, such as optical clearing or mechanical compression. Table I summarizes reported studies on OCT gynecologic applications, advantages, and drawbacks for every particular application and achieved sensitivity and specificity, where applicable.

The overviewed OCT applications in gynecology indicate high potential of this technique in treatment monitoring; however, no such gynecologic applications were reported so far. Recently, OCT was reported as an efficient tool for treatment monitoring of skin and mucous tissues of other localizations. One of the modern trends in gynecology is the use of organ-preserving treatment approaches, in particular, PDT. Demonstrated capabilities of OCT in the detection of morphological alterations can be employed for monitoring PDT of gynecologic localizations for treatment optimization and personalization. Additional advantages in diagnostic accuracy can be provided by advanced OCT modalities, such as polarization-sensitive OCT, providing information about birefringent

![Fig. 2 Typical OCT images and corresponding histology of fallopian tube tissue: (a, d) norm, (b, e) inflammation with prevalence of edema, and (c, f) chronic alterations with fibrosis.](image-url)
<table>
<thead>
<tr>
<th>Clinical problem</th>
<th>Methods</th>
<th>Sensitivity/specificity</th>
<th>Advantages</th>
<th>Drawbacks</th>
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<tbody>
<tr>
<td><strong>Diagnostics of cervical cancer</strong></td>
<td>\textit{In vivo} OCT\textsuperscript{16,35}</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. OCT increases specificity of colposcopy</td>
<td>High requirements to probe sterilization to avoid virus contamination or requirement for employment of disposable probes or probe holders. Requirement for special holders for fiber-optics probes to reach the inspection site.</td>
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<td></td>
<td>\textit{In vivo} OCT\textsuperscript{38}</td>
<td>Detection of $\geq$CIN II 95(96)%/46(29)%</td>
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<td></td>
<td>\textit{In vivo} OCT\textsuperscript{39}</td>
<td>Detection of $\geq$CIN II 86 (84)%/64 (60)%</td>
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<td></td>
<td>\textit{In vivo} OCT + numerical processing\textsuperscript{36}</td>
<td>n/a</td>
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<td></td>
<td>\textit{In vivo} OCT + VIA + colposcopy\textsuperscript{37}</td>
<td>Detection of $\geq$CIN II VIA 76%/34%</td>
<td>OCT+VIA 53%/61%</td>
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<td></td>
<td></td>
<td></td>
<td>OCT + VIA + colposcopy 46%/69%</td>
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<td></td>
<td>\textit{In vivo} OCT+VIA\textsuperscript{40}</td>
<td>Detection of $\geq$CIN II 62%/80%, $n=1000$</td>
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<td></td>
<td>\textit{In vivo} OCT + colposcopy\textsuperscript{41}</td>
<td>Detection of $\geq$CIN II</td>
<td>Colposcopy 60%/83%</td>
<td></td>
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<td></td>
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<td></td>
<td>OCT + colposcopy 29%/93%, $n=299$</td>
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<td></td>
<td>\textit{Ex vivo} OCT + microscopy\textsuperscript{25}</td>
<td>Detection of $\geq$CIN II 88(84)%/69(65)%, $n=20$</td>
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<td>\textit{In vivo} PS OCT\textsuperscript{49}</td>
<td>n/a</td>
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<td><strong>Diagnostics of vulvar cancer</strong></td>
<td>\textit{In vivo} OCT\textsuperscript{43,44}</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. No special requirements to OCT probe geometry.</td>
<td>High requirements to probe sterilization to avoid virus contamination or requirement for employment of disposable probes or probe holders. Requirement for numerical processing, no evident visual criteria.</td>
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<td></td>
<td>\textit{In vivo} OCT + calculation of epidermal thickness\textsuperscript{36}</td>
<td>Detection of VIN/VSCC 100%/80%</td>
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<td></td>
<td>\textit{In vivo} OCT + calculation of attenuation coefficient\textsuperscript{45}</td>
<td>Detection of VIN/VSCC 100%/70%</td>
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<tr>
<td><strong>Diagnostics of ovarian cancer</strong></td>
<td>\textit{In vivo} laparoscopic OCT\textsuperscript{49}</td>
<td>n/a</td>
<td>In addition to basic laparoscopy procedure, OCT provides noninvasive real-time structure imaging.</td>
<td>OCT probe should be compatible with a laparoscopic trocar. Ovary anatomy (protein cover) complicates imaging of the ovary inner structure.</td>
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<tr>
<td></td>
<td>\textit{In vivo} OCT+PAI+US\textsuperscript{54}</td>
<td>n/a</td>
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<td></td>
<td>\textit{Ex vivo} OCT + positron detection\textsuperscript{55}</td>
<td>n/a</td>
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<td></td>
<td>\textit{Ex vivo} OCT + calculation of attenuation coefficient\textsuperscript{52}</td>
<td>Detection of ovary cancer 80(61)%/75(90)%</td>
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<td>\textit{Ex vivo} OCT + angle-resolved calculation of attenuation coefficient\textsuperscript{51}</td>
<td>Detection of ovary cancer 100% /100%, $n=10$</td>
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<td></td>
<td>\textit{Ex vivo} PS OCT+calculation of scattering coefficient\textsuperscript{52}</td>
<td>Detection of ovary cancer 43% /100%</td>
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<td></td>
<td>\textit{Ex vivo} full-field OCT + image processing\textsuperscript{56,59}</td>
<td>Detection of ovary cancer 92% /88%</td>
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properties of tissues and OCT-angiography allowing for high-resolution mapping of microcirculation within tissues.

Disclosures
The authors have nothing to disclose.

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References

Table 1 (Continued).

<table>
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<tr>
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<th>Sensitivity/specificity</th>
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<th>Drawbacks</th>
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</thead>
<tbody>
<tr>
<td>Diagnostics of endometriosis</td>
<td><em>Ex vivo</em> OCT&lt;sup&gt;19&lt;/sup&gt;</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. High potential in differential diagnostics of small types of endometriosis.</td>
<td>OCT probe should be compatible with a laparoscopic trocar. Too little observations reported.</td>
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<td></td>
<td><em>In vivo</em> OCT&lt;sup&gt;60&lt;/sup&gt;</td>
<td>n/a</td>
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<td>Diagnostics of fallopian tubes disorders</td>
<td><em>In vivo</em> OCT + laparoscopy + numerical processing&lt;sup&gt;61&lt;/sup&gt;</td>
<td>Detection of salpingitis Laparoscopy 44%/67% OCT + laparoscopy 90%/81% OCT + laparoscopy + numerical processing 100%/98%, n = 61</td>
<td>Noninvasive real-time diagnostics. Unique ability to obtain <em>in vivo</em> information on structure of muscular layer of a fallopian tube. Additional information for differential diagnostics of morphological forms of inflammatory diseases.</td>
<td>OCT probe should be compatible with a laparoscopic trocar.</td>
</tr>
<tr>
<td>Diagnostics of endometritis</td>
<td><em>In vivo</em> OCT + numerical processing&lt;sup&gt;62,63&lt;/sup&gt;</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. Additional information for differential diagnostics of morphological forms of inflammatory diseases.</td>
<td>OCT probe should be compatible with a hysteroscope, incompatibility with office-based hysteroscope.</td>
</tr>
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<td>Diagnostics of nonmalignant cervix alterations</td>
<td><em>In vivo</em> OCT&lt;sup&gt;16,25,36&lt;/sup&gt;</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. Additional information for differential diagnostics of morphological forms of inflammatory diseases.</td>
<td>High requirements to probe sterilization to avoid virus contamination or requirement for employment of disposable probes or probe holders. Requirement for special holders for fiber-optics probes to reach the inspection site.</td>
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<td>Diagnostics of vaginal epithelial damage</td>
<td><em>In vivo</em> OCT + vulvoscopy&lt;sup&gt;64,65&lt;/sup&gt;</td>
<td>n/a</td>
<td>Noninvasive real-time diagnostics. No special requirements to OCT probe design. Additional information for differential diagnostics of morphological forms of inflammatory diseases.</td>
<td>High requirements to probe sterilization to avoid virus contamination or requirement for employment of disposable probes or probe holders.</td>
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</table>

Note: OCT, optical coherence tomography; PS OCT, polarization-sensitive OCT; VIA, visual inspection with acetic acid; CIN, cervical intraepithelial neoplasia; VIN, vulvar intraepithelial neoplasia; VSCC, vulvar squamous cell carcinoma; PAI, photoacoustic imaging; and US, ultrasound. In the brackets, alternative reported value is shown.

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