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Abstract. A clinical validation of the bone scan lesion area (BSLA) as a quantitative imaging biomarker was performed in metastatic castration-resistant prostate cancer (mCRPC). BSLA was computed from whole-body bone scintigraphy at baseline and week 12 posttreatment in a cohort of 198 mCRPC subjects (127 treated and 71 placebo) from a clinical trial involving a different drug from the initial biomarker development. BSLA computation involved automated image normalization, lesion segmentation, and summation of the total area of segmented lesions on bone scan AP and PA views as a measure of tumor burden. As a predictive biomarker, treated subjects with baseline BSLA <200 cm² had longer survival than those with higher BSLA (HR = 0.4 and p < 0.001). As a surrogate outcome biomarker, subjects were categorized as progressive disease (PD) if the BSLA increased by a prespecified 30% or more from baseline to week 12 and non-PD otherwise. Overall survival rates between PD and non-PD groups were statistically different (HR = 0.64 and p = 0.007). Subjects without PD at week 12 had longer survival than subjects with PD: median 398 days versus 280 days. BSLA has now been demonstrated to be an early surrogate outcome for overall survival in different prostate cancer drug treatments. © The Authors. Published by SPIE under a Creative Commons Attribution 3.0 Unported License. Distribution or reproduction of this work in whole or in part requires full attribution of the original publication, including its DOI.

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1 Introduction

More than 90% of patients with advanced prostate cancer develop bone metastases,¹ which can produce some of the most severe complications of the disease and is associated with shorter survival times.¹ New drugs are under development for metastatic castration-resistant prostate cancer (mCRPC), and there is a need for biomarkers to identify target populations and for early evaluation of treatment effects as an alternative to overall survival, which leads to long studies and is becoming problematic due to subject crossover and contamination from multiple therapies.

Whole-body bone scintigraphy is the accepted standard imaging modality for detection of bone metastases and assessment of treatment outcomes. Response evaluation criteria in solid tumors, the standard guideline used to assess outcomes in solid tumor malignancies, treats bone lesions as “nonmeasurable” and is therefore of limited usefulness in the setting of prostate cancer treatments.¹ Therefore, the Prostate Cancer Working Group 2 (PCWG2) developed visually based criteria for assessing disease progression on bone scans based on counting new lesions.² PCWG2 does address the significance of changes in intensity, size, or area of individual lesions, all of which are limited by the challenges of subjective, visual lesion detection.

The simple conventional metric of lesion counting is of limited value when assessing treatment effects, as lesions may decrease in size without changing in number or may break into smaller components and, thus, superficially appear as an increased metastatic burden. This motivated the development of computer-aided quantitative measures of disease burden on bone scans.

The two quantitative bone imaging biomarkers that have undergone the most study and use in oncologic clinical trials are the bone scan index (BSI)³ and bone scan lesion area (BSLA).⁴ The BSI sums the product of the estimated weight and the fractional involvement of each bone, determined visually or from lesion segmentation on the bone scan. BSI was first evaluated as a prognostic biomarker⁴ and has had a number of more recent follow-up studies.⁵ BSLA was the first quantitative imaging biomarker to be developed and evaluated primarily for treatment response assessment in prostate cancer. The calculation and its ongoing clinical validation will be described in this paper.

In development of an imaging biomarker, there are two important phases: (1) development and analytic validation (including training of classifiers, determination of cut points, assessment of reproducibility, and evaluation against radiologist measurements) and (2) clinical validation in which the system and its cut points are fixed and it is evaluated against outcomes in new clinical trial data. BSLA is an imaging biomarker computed from whole-body scintigraphic imaging as a measure
of overall bone tumor burden. Initial development and analytic validation, including evaluation against manual tumor segmentation and determination of response thresholds using trial cohorts, are from a single drug treatment (cabozantinib) with controls in subjects with metastatic CRPC. A 30% increase/decrease in BSLA relative to baseline was defined as progression/response on bone scan based on the data from these previous cohorts. Because of the promising results and urgent need, the BSLA imaging biomarker was rapidly adopted in clinical trials, such as using the drug for which the biomarker was initially developed and, in Ref. an ongoing trial using a different treatment. Therefore, rather than an investigation into threshold or other algorithm parameters, this paper is focused on clinical validation of an existing test that has been adopted by the research community in prostate cancer clinical trials. In the computer-aided diagnosis research community, the majority of papers involve analytic validation, and this clinical validation is the next step in putting biomarker translation into practice. As a clinical validation, the analysis approach in this paper is consistent with those used in clinical trials.

We hypothesize that, when applied to an independent treatment trial cohort with a different mechanism of drug action, a week 12 change posttreatment using this prespecified threshold for progression is predictive of a subject’s overall survival, i.e., can be used as a surrogate outcome marker. Second, we evaluated the potential of baseline BSLA (disease burden on the baseline scan) as a predictive biomarker used to identify patients most likely to benefit from treatment.

2 Methods

2.1 Data Collection

From an anonymized imaging research database, a cohort of 198 mCRPC subjects who enrolled in a multicenter treatment trial of abiraterone acetate (127 treated and 71 placebo) using a standardized imaging protocol was identified. Subjects were included that had whole-body original DICOM images and survival data available. This cohort was independent of those used for development of the biomarker criteria for progression/response and involved a different mechanism of drug action. Subjects underwent the standard of care whole-body bone scintigraphy with 99mTc-Methyl diphosphonate (99mTc-MDP) at baseline and week 12 posttreatment.

2.2 Bone Scan Image Processing

A CADrx system for bone scan assessment was developed within the imaging biomarker information system (IBIS) for image markup and analysis (MedQIA, LLC, Los Angeles, California). The IBIS markup system combines image review capabilities with computer-aided tools for region segmentation, quantitative analysis, and data export for clinical trials. In the CADrx system, anterior and posterior bone scan images are processed with pixel intensity normalization and lesion segmentation, followed by quantitative assessment of lesion burden. The image analysis method was previously described in detail and the steps are summarized here.

2.2.1 Anatomical region segmentation

Atlas-based segmentation was performed to label seven anatomical regions on the bone scan: sternum/spine, ribs/head, extremities (arms and legs), pelvis, shoulders, kidney search region, and bladder search region. Registration to the atlas involved affine registration using the Mattes mutual information metric followed by a multiresolution demons deformable registration. An example of the output of the anatomical region segmentation is shown in Fig. 1.

Fig. 1 Automated anatomical region segmentation of ribs/head (red), spine/sternum (yellow), pelvis (green), extremities (blue), shoulders (magenta), kidney search region (cyan), and bladder search region (orange).
2.2.2 Image intensity normalization

Image intensity normalization was applied to reduce inter- and intrapatient variations due to differences in body habitus, radiotracer dosing levels, and scan acquisition parameters. A region of normal bone in the extremities was identified automatically based on the anatomical region segmentation. Then all pixel values were linearly rescaled to set the intensity of this normal bone to a reference intensity. After normalization, the pixel intensities of normal bone are consistent between subjects and across time points for a given subject, allowing for reproducible lesion segmentation and quantitative assessment in serial patient images.

2.2.3 Automated lesion detection

Based on the atlas-based segmentation, anatomical region-specific lesion intensity thresholds for lesion detection were learned previously using receiver operating characteristic (ROC) analysis on a training set of images. The ROC analysis was used to set the region-specific thresholds to maximize segmentation accuracy against expert delineated reference segmentations on the training set. An additional classification stage was applied to candidate lesions generated by the thresholding to remove false positives related to bladder uptake, kidney uptake, and symmetric degenerative joint disease. False positives related to uptake in these anatomical regions were identified and removed based on overlap with corresponding regions from the atlas-based segmentation. Symmetric degenerative joint disease removal involved computing features of lesion candidates: lesion area, mean intensity, perpendicular distance from the midline, and vertical distance along the midline. Lesion candidates were compared in a pairwise manner and symmetric pairs identified based on feature difference thresholds. Parameters in the false positive reduction were trained using a multistart local optimization method using the Nelder–Mead simplex.

2.2.4 Segmentation review and approval

For each bone scan, the results of the automated lesion segmentation were reviewed by a nuclear medicine physician and manually edited (lesion pixels added or removed) as needed. This editing typically involved removal of any remaining false-positive regions (e.g., areas of degenerative joint disease) and took on the order of minutes per scan. Previous studies showed 89% pixel accuracy of the lesion segmentation method against manual expert annotations, so the amount of editing required for a given case is typically minimal.

2.3 Treatment Response Assessment Using Bone Scan Lesion Area

BSLA is summed as $\text{BSLA} = \sum_{p \in R} A_p$, where $R$ is the set of pixels identified as bone lesion and $A_p$ is the physical area of pixel $p$ (in cm$^2$). The BSLA measure thus represents a quantification of the size and number of active regions on the bone scan. BSLA was calculated at baseline and week 12 posttreatment for all subjects in the study. A prespecified 30% increase in BSLA from baseline to week 12 was used to identify subjects with progressive disease (PD). Subjects with <30% increase or decrease in BSLA were categorized as nonprogressive disease (non-PD). For evaluation as a prognostic factor, the dataset was dichotomized about the median baseline BSLA. Figure 2 shows examples of bone scans with lesions semiautomatically segmented in red and changes in BSLA computed from baseline to week 12. The examples reflect PD (an increase in lesion burden) and non-PD (stable and reduction in lesion burden).

2.4 Statistical Analysis

BSLA was evaluated as a prognostic factor, predictive biomarker, and a surrogate outcome biomarker. Subjects were grouped as PD versus non-PD and multivariate Cox regression was used to test whether (1) baseline BSLA and (2) early

![Fig. 2 Example cases with lesions segmented in red and BSLA change assessment.](https://www.spiedigitallibrary.org/journals/Journal-of-Medical-Imaging)
changes in BSLA (12 weeks posttreatment) were predictive of overall survival. Landmark survival analyses were used to assess early changes. Kaplan–Meier plots and hazard ratios were used to evaluate differences among groups defined by the BSLA biomarker.

3 Results

3.1 Prognostic and Predictive Biomarker Evaluation

Median BSLA at baseline was 219 cm². BSLA <200 cm² at baseline was a prognostic factor for delaying progression (HR = 0.6 and \( p = 0.003 \)) and predictive of longer survival (HR = 0.4 and \( p < 0.001 \)). Figure 3 shows Kaplan–Meier plots of the proportion of subjects surviving a given number of days beyond baseline when separated into groups based on the baseline BSLA score.

Figure 3(b) shows BSLA as a predictive factor including all subjects, both treatment and control groups. It shows that subjects with low baseline BSLA scores (<200 cm²) have a better overall prognosis across all treatment groups. BSLA scores undergoing treatment (<200 cm²) can be predicted to have a better survival outcome than those with high BSLA scores. Subjects with low baseline BSLA scores have a relatively good overall prognosis, irrespective of whether they are treated (blue and black survival curves).

3.2 Early Surrogate Outcome Evaluation

Overall survival rates between PD and non-PD groups were statistically different (HR = 0.64 and \( p = 0.007 \)). Subjects without PD by BSLA at week 12 had longer survival than subjects with PD: median 398 days versus 280 days (378 days versus 228 days after adjustment for baseline BSLA <200 cm²). Similar differences were seen within the treatment and placebo groups (see Table 1). The corresponding Kaplan–Meier survival curves are shown in Fig. 4, and multivariate Cox regression analysis for survival is shown in Table 2.

4 Discussion

As a prognostic and predictive biomarker, the BSLA can facilitate patient management and prospective determination of those most likely to benefit from a given therapy, rather than beginning a therapy and waiting months to see if the disease progresses or not, which is particularly problematic for advanced prostate cancer. Specifically, subjects with high BSLA should be treated (low BSLA has a relatively good prognosis regardless of whether treated or not). In addition to using the median baseline

Table 1 Median survival in days after week 12, with number of subjects in each group (adjusting for baseline BSLA score <200 cm²).

<table>
<thead>
<tr>
<th></th>
<th>PD by BSLA</th>
<th>Non-PD by BSLA</th>
</tr>
</thead>
<tbody>
<tr>
<td>Placebo group</td>
<td>186 (±221) days</td>
<td>170 (±222) days</td>
</tr>
<tr>
<td>(N = 45)</td>
<td></td>
<td>(N = 26)</td>
</tr>
<tr>
<td>Treatment group</td>
<td>260 (±254) days</td>
<td>392 (±311) days</td>
</tr>
<tr>
<td>(N = 65)</td>
<td></td>
<td>(N = 61)</td>
</tr>
<tr>
<td>All</td>
<td>228 (±242) days</td>
<td>378 (±327) days</td>
</tr>
<tr>
<td>(N = 111)</td>
<td></td>
<td>(N = 87)</td>
</tr>
</tbody>
</table>

Fig. 3 Kaplan–Meier plots for low BSLA (<200 cm²) versus high BSLA (> = 200 cm²) as (a) prognostic factor and (b) predictive biomarker.

Fig. 4 Survival plots for non-PD versus PD by BSLA at week 12 in control (placebo) and treatment groups after adjustment of baseline BSLA score <200 cm².
BSLA (50th centile) as a prognostic cut point, we performed a sensitivity analysis by testing the 33rd and 67th points for BSI groupings being explored rather than prespecified. In a mCRPC cohort, Reza et al. found that an increase in BSI at follow up of at most 0.30 had a significantly longer median survival time than those with an increase of BSI >0.30. They note that retrospective design (choice of BSI cut point) was a limitation. In another mCRPC cohort in which a different cut point of not >20% increase from BSI baseline was applied, they found that the group had a significantly longer time to progression in bone than those who had a BSI increase >20% during treatment. These studies differ from ours in that we prespecified the criteria for disease progression of 30% or more increase in BSLA and then applied it prospectively to this and other new cohorts to demonstrate robustness across different therapeutic protocols.

The focus of this paper has been on clinical validation of an existing algorithm already adopted in trials. However, as more data are becoming available, there will be an opportunity to update parameters in the algorithm, such as the intensity thresholds and response/progression cut points, and to include more advanced classifiers to further improve performance. For example, the currently used 30% cut point for progression/response was set conservatively in a small developmental set such that all control subjects had BSLA changes less than this threshold and, as further reproducibility studies are performed, we may be able to reduce the threshold and increase the sensitivity of the biomarker. Because the initial developmental set was relatively small, the subsequent larger clinical validation studies, such as Ref. and this one in a different drug treatment, are particularly important to show that the current algorithm in use in clinical trials provides an effective surrogate for overall survival.

Table 2 Multivariate Cox regression for survival.

<table>
<thead>
<tr>
<th>Coefficient</th>
<th>HZ (±SE)</th>
<th>p-value</th>
<th>95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td>Treatment</td>
<td>0.49 (±0.11)</td>
<td>0.002</td>
<td>[0.32, 0.76]</td>
</tr>
<tr>
<td>Baseline BSLA &lt;200 cm²</td>
<td>0.34 (±0.09)</td>
<td>&lt;0.001</td>
<td>[0.20, 0.58]</td>
</tr>
<tr>
<td>Interaction between treatment and BSLA</td>
<td>2.15 (±0.70)</td>
<td>0.019</td>
<td>[1.14, 4.08]</td>
</tr>
<tr>
<td>Non-PD</td>
<td>0.64 (±0.11)</td>
<td>0.007</td>
<td>[0.46, 0.88]</td>
</tr>
</tbody>
</table>

BSLA is calculated semiautomatically from bone scans and provides a quantitative and objective treatment response assessment. Baseline BSLA and early changes posttreatment were found to be predictive of overall survival in patients with mCRPC. BSLA has now been demonstrated to be an early surrogate outcome for overall survival in different prostate cancer drug treatments.

5 Conclusion

BSLA is calculated semiautomatically from bone scans and provides an early surrogate for overall survival in different prostate cancer treatments.

Disclosures

Conflict of interest disclosure: Matthew S. Brown and Jonathan G. Goldin are directors of MedQIA Imaging CRO.

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References


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