Extraction of depth-dependent signals from timeresolved reflectance in layered turbid media

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1 Introduction

Near-infrared spectroscopy (NIRS) has often been used for noninvasive evaluation of tissue oxygenation. Recently, this technique has been developed as a tool for human brain mapping by measuring the hemodynamic changes of cerebral cortex associated with neuronal activation.1-3 NIRS has some advantages over other methods for cerebral hemodynamics evaluation such as positron emission tomography (PET) and functional magnetic resonance imaging (fMRI) in terms of, for example, temporal resolution, easier handling, and less motion restriction during measurement. Some problems, however, remain to be solved before the application of NIRS to measurements of the human head. The head is a layered structure consisting of cerebral and extracerebral tissues (scalp, skull, and cerebrospinal fluid), and each layer has different optical properties. When light is applied to the scalp and diffusely reflected light is collected at a position on the scalp a few centimeters away from the incident point, the detected light carries information concerning not only the cerebral but also extracerebral tissues. Because the changes in extracerebral blood flow influence the determination of cerebral hemoglobin (Hb) concentration changes, some reports⁴⁻⁶ have questioned the validity of cerebral NIRS. It is thus necessary to separate signals originating in the cerebral tissue from

Abstract. We try a new approach with near-IR time-resolved spectroscopy, to separate optical signals originated in the upper layer from those in the lower layer and to selectively determine the absorption coefficient (μ_a) of each layer in a two-layered turbid medium. The difference curve in the temporal profiles of light attenuation between a target and a reference medium is divided into segments along the time axis, and a slope of each segment is calculated to determine the depth-dependent μ_a . The depth-dependent μ_a values are estimated under various conditions in which μ_a and the reduced scattering coefficient (μ'_{c}) of each layer are changed with a Monte Carlo simulation and in phantom experiments. Temporal variation of them represents the difference in μ_a between two layers when μ'_s of a reference is the same as that of the upper layer of the target. The discrepancies between calculated μ_a and the real μ_a depend on the ratio of the real μ_a of the upper layer to that of the lower layer, and our approach enables us to estimate the ratio of μ_a between the two layers. These results suggest the potential that μ_a of the lower layer can be determined by our procedure. © 2005 Society of Photo-Optical Instrumentation Engineers. [DOI: 10.1117/1.2136312]

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those in the extracerebral tissue. As one of the ways for this purpose, a multidetector system consisting of continuouswave-type (cw-type) instruments has been developed.^{7,8} In this approach, however, separation of NIR signals attributed to cerebral and extracerebral tissues was incomplete because the measurement by different distances of light guide pairs might cause a discrepancy in the position where signals originate. In addition, with instruments of this type, it was difficult to quantify the Hb concentration.^{9,10} The absolute value of Hb concentration is indispensable because neuronal activation and hemodynamic changes seem to significantly depend on the baseline conditions,^{11,12} and also to compare the magnitude of the changes between different cortical areas and/or individuals.

In contrast, time-resolved reflectance measurement with short-pulsed light [time-resolved spectroscopy (TRS)], which gives a temporal profile of detected light intensity, has high potential to overcome these issues. It is believed to carry information about depth-dependent attenuation based on the correlation of detection time to penetration depth of photons.^{13–17} Furthermore, it makes possible the determination of the optical properties in turbid media such as the absorption coefficient^{18,19} (μ_a) of which acquisition at multiple wavelengths can give quantitative Hb concentrations. In most cases of conventional TRS measurements for the human head, μ_a was determined by fitting an analytical solution of the

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photon diffusion equation for a homogenous medium to the time-resolved reflectance profile on the assumption that the target medium is a semiinfinite homogeneous. The analysis based on this assumption not only causes an error in estimation of the optical properties of the human head²⁰⁻²⁴ but also cannot bring out the depth-dependent information. Therefore, new analytical methods that are suitable for layered media are required. To overcome this problem, some methods have been provided, such as by multilayered (time-dependent) diffusion equation^{9,25-27} and by moments of distribution of time of flight.^{16,28} Most of these analyses are employed by combination with the measurements at two or more distances, whereas a single-distance measurement is more favorable for practical measurements on the head due to the heterogeneity of the superficial layer and its curvature. On the other hand, the analysis with time-dependent mean partial path length by Steinbrink et al.¹⁶ could be applied to a single-distance measurement, but it did not enable us to estimate μ_a in a given condition but only the change in μ_a from one condition to another.

In this paper, we attempt to develop a simple analytical method to separate optical signals originated in shallower layers from those in deeper layers and to selectively determine the μ_a values of them by TRS measurements with a single fixed source-detector spacing. As the first step of an analysis of a multilayer model such as the human head, a two-layered medium was considered. Our approach to this purpose is "time-segment analysis," which divides the temporal profile of detected light intensity into time segments (e.g., every 500 ps), leading to an estimation of depth dependent μ_a . In this paper, we first demonstrate μ_a estimated by the slope of each time segment (time-segmented μ_a) and its discrepancy from the real μ_a of the lower layer under various conditions in which μ_a and reduced scattering coefficient (μ'_s) of each layer were changed with a Monte Carlo simulation and in phantom experiments. We also show the relationship between such discrepancy and the difference in μ_a between the upper and lower layers. Then we discuss a correction of timesegmented μ_a that was estimated smaller than the real μ_a with the ratio of time-segmented μ_a in an earlier time segment to that in a later one. In addition, we consider a way to calculate an appropriate μ_a in the case that μ'_s of medium was unknown. Finally, we suggest the applicability of our approach in practical measurement.

2 Method for Determining μ_a

2.1 Theoretical Consideration

When a light impulse is incident on the surface of a semiinfinite homogeneous medium (object), the time-resolved intensity of reflected light at time *t* can be expressed as²⁹

$$I(t) = S(t)\exp(-\mu_a ct), \qquad (1)$$

where μ_a is the absorption coefficient of the medium, *c* is the light velocity in the medium, and *S*(*t*) is a scattering function that is dependent on their reduced scattering coefficient (μ'_s) in the photon diffusion regime. We consider a reference medium besides the object. The reflected light intensity for the reference at *t* is written as $I_R(t)=S_R(t)\exp(-\mu_{a,R}c_Rt)$, where the subscripts *R* to *I*(*t*), μ_a , *c*, and *S*(*t*) indicate a reference.



Fig. 1 Number of scattering events in the upper part of the depth from 2 to 36 mm for a homogeneous semiinfinite medium ($\mu_a = 0 \text{ mm}^{-1}$, $\mu'_s = 1.0 \text{ mm}^{-1}$, $\rho = 30 \text{ mm}$, n = 1.37), predicted by Monte Carlo simulation. The vertical axis represents the number of scattering events per photon detected at time *t*.

Attenuation (A) is defined as logarithm of the inverse of reflectance and according to the time-resolved Beer-Lambert law,³⁰ difference between the attenuation of an object [A(t)]and that of a reference $[A_R(t)]$, $A^{\text{diff}}(t)$, can be expressed as

$$A^{\text{diff}}(t) = A(t) - A_R(t) = \ln[I_R(t)/I(t)] = (\mu_a c - \mu_{a,R} c_R)t + S^{\text{diff}}(t),$$
(2)

where $S^{\text{diff}}(t) = \ln [S_R(t)/S(t)]$. When μ'_s and the refractive index are the same for the reference and the object, $S^{\text{diff}}(t)$ vanishes and $A^{\text{diff}}(t)$ becomes linear to t and its slope is denoted as $\mu_a^{\text{diff}}c$, where $\mu_a^{\text{diff}} = \mu_a - \mu_{a,R}$, and $c = c_R$. However, in the case where the object is an inhomoge-

However, in the case where the object is an inhomogeneous medium (and the reference is a homogeneous one), $A^{\text{diff}}(t)$ is no longer linear to t even if $S^{\text{diff}}(t)$ can be ignored. When μ_a^{diff} varies due to the layer structure, $dA^{\text{diff}}(t)/dt$ reflects the depth dependence in μ_a^{diff} . Here we introduce time-dependent apparent absorption coefficient, $\mu_a(t)$, given by $\sum_i \mu_{ai} l_i(t)/L(t)$, where the subscript *i* refers to the layer number in the object medium, $l_i(t)$ is the mean partial path length in the *i*'th layer for the photons detected at time *t*, and L(t) is total path length defined as L(t) = ct. Then we define time dependent difference in apparent absorption coefficient $\mu_a^{\text{diff}}(t)$, which is the difference between $\mu_a(t)$ and $\mu_{a,R}$ at each time. In the case of two-layered media, the *i*'th layer simply corresponds to either upper or lower layer and $dA^{\text{diff}}(t)/dt$ is expressed as follows:

$$dA^{\text{diff}}(t)/dt = (d/dt) [\mu_a^{\text{diff}}(t)ct] + dS^{\text{diff}}(t)/dt$$
$$= \mu_{a,\text{upper}} [dl_{\text{upper}}(t)/dt] + \mu_{a,\text{lower}} [dl_{\text{lower}}(t)/dt]$$
$$- \mu_{a,R}c + dS^{\text{diff}}(t)/dt, \qquad (3)$$

where $\mu_{a,\text{upper}}$ and $\mu_{a,\text{lower}}$ are the μ_a values of the upper and lower layer for an object, and $l_{\text{upper}}(t)$ and $l_{\text{lower}}(t)$ are the mean partial path length in the upper and lower layers at time *t*, respectively. Figure 1 shows time dependence of the number of scattering events for the photons detected by reflectance mode in the upper part of the depth from 2 to 36 mm for a homogeneous semiinfinite medium ($\mu_a = 0 \text{ mm}^{-1}$, μ'_s = 1.0 mm⁻¹, source-detector distance $\rho = 30 \text{ mm}$, n = 1.37), predicted by a Monte Carlo simulation. As for photons detected later in time in the measurement of reflectance mode, the number of scattering events in shallow layers is almost constant. This is typically seen after around 3 ns in layers that are shallower than 10 mm. Because the number of scattering events is converted to the photon path length by mean free pass, the mean partial path lengths of the shallow layers can be considered constant after 3 ns. At a later time, therefore, the mean partial path length in deeper layers is dominant to the total path length.

2.2 Time-Segmented μ_a and Method for Obtaining μ_a of the Lower Layer

Next, we introduced mean absorption differences obtained by $\Delta A^{\text{diff}}(t)/\Delta t$ instead of $dA^{\text{diff}}(t)/dt$ in consideration of errors by getting the regression curve and to simplify an analysis process. For this aim, we divided the temporal profile of detected light intensity into segments to extract time-dependent μ_a (time-segment analysis). When we assume that μ'_s and refractive index are the same for reference and object,

$$\Delta A^{\text{diff}}(t) / \Delta t = (1/\Delta t) (\mu_{a,\text{upper}} \Delta l_{\text{upper}}(t) + \mu_{a,\text{lower}} \Delta l_{\text{lower}}(t) - \mu_{a,R} c \Delta t) = \{\mu_{a,\text{upper}} [\Delta l_{\text{upper}}(t) / \Delta L(t)] + \mu_{a,\text{lower}} [\Delta l_{\text{lower}}(t) / \Delta L(t)] \} c - \mu_{a,R} c, \quad (4)$$

where $\Delta L(t)$ is total path length change, which is $\Delta l_{upper}(t) + \Delta l_{lower}(t) = c \Delta t$. As shown in Fig. 1, if $\Delta l_{upper}(t)$ is negligible after 3 ns, the slopes of $A^{diff}(t)$ against ct at later time segments converge to $(\mu_{a,lower} - \mu_{a,R})$. If we know $\mu_{a,R}$, $\mu_{a,lower}$ can thus be determined. We refer to $\{\mu_{a,upper}[\Delta l_{upper}(t)/\Delta L(t)] + \mu_{a,lower}[\Delta l_{lower}(t)/\Delta L(t)]\}$ as the time-segmented μ_a, μ_a^{seg} , which represents a depth-dependent absorption coefficient at each time segment. It depends on the contribution of the change in the mean partial path length to that in the total path length between two different times. Accordingly, Eq. (4) could be rewritten again as $\Delta A^{diff}(t)/\Delta t = (\mu_a^{seg} - \mu_{a,R})c$.

In the following, a calculation process is explained for the case of the two-layered object and homogeneous reference. First, from the two sets of data for the object and reference, we calculate $A^{\text{diff}}(t)$ profile and divide it into segments. Then $A^{\text{diff}}(t)$ at each time segment is approximated linear to time and its slope (time-segmented slope) is estimated by linear regression. From the time-segmented slope, μ_a^{seg} can be obtained from $\mu_{a,R}$ and c based on Eq. (4). In this study, time range of 500 ps was selected for the segment size considering the reliability of regression analysis of the time-segmented slope. Before calculations of $A^{\text{diff}}(t)$, temporal profiles of light intensity measured by TRS are deconvoluted by the pulse response of the system that can be determined in every experiment. Deconvolution can be performed by the Fourier transform, and higher frequency components over 3/4 of the maximum are eliminated as they are judged to be noise.

3 Simulation and Experiment

3.1 Monte Carlo Simulation

To analyze the light propagation and calculate the reflectance from a two-layered semiinfinite medium, we used the Monte Carlo code developed by Wang and Jacques.³¹ The code was modified to correspond to our measurement system. The number of scattering events in layers ranging from z to z+2 mm in depth, and reflectance for the medium were calculated with the time step of 10 ps. Source photons were perpendicularly irradiated on the surface of the semiinfinite media, and photons that were emitted from a detector position on the surface were all detected. The source-detector distance was 30 mm. The calculation was repeated until the number of the detected photons reached 1,000,000. For each layer separately, μ'_{s} were given as 1.0 and 1.5 mm⁻¹ and μ_a were varied at the range of 0.005 to 0.02 mm⁻¹. These values were chosen close to the optical properties of the tissues in human heads, μ'_s and μ_a of the head³² were 0.7 to 1.0 and 0.012 to 0.016 mm⁻¹ at 825 nm, and μ'_s and μ_a of gray matter³³ were 0.4 to 0.7 and 0.018 mm⁻¹ at 849 nm, respectively. To compare with the results of phantom experiments described in the following, a case for smaller μ_a value (0.005 mm⁻¹) was also examined. We compared some reflectance profiles simulated in an anisotropic setting (scattering coefficient $\mu_s = 10 \text{ mm}^{-1}$, anisotropy parameter g = 0.9) with those in an isotropic one ($\mu'_s = 1.0 \text{ mm}^{-1}$) and confirmed that the difference between the two was small enough to be ignored. Therefore, isotropic scattering was assumed to reduce the calculation time. A refractive index of 1.37 was used for both the upper and lower layers.

3.2 Phantom Preparation

Homogeneous and two-layered gelatin phantoms, the sizes of which were $230 \times 230 \times 55$ to 70 mm, were prepared. The thicknesses of the upper layers in two-layered phantoms were 10 and 15 mm. The base material of phantoms was an 8 wt% gelatin (Wako Pure Chemical Industries, Ltd., Osaka, Japan) solution. The gelatin solution itself was transparent and its μ_a is 0.003 mm $^{-1}$ at 760 nm. We adjusted μ_s' and μ_a to 1.0 to 1.5 and 0.003 to 0.02 mm⁻¹ at 760 nm, respectively, by adding Intralipid (Fresenius Kabi AB, Upsala, Sweden) as scatterers and ink (greenish brown ink; Chugai Kasei Co., Musashino, Japan; μ_a at 760, 800, and 830 nm were 0.247, 0.180, and 0.125 mm⁻¹, respectively, in 1 vol% aqueous solution) as an absorber. A homogeneous phantom without ink $(S0; \mu'_{s} = 1.0 \text{ mm}^{-1}, \mu_{a} = 0.003 \text{ mm}^{-1})$ was also prepared as a reference for analysis. We determined μ_s' and μ_a of each phantom by curve fitting the solution of photon diffusion equation to time-resolved data (the details are described in Sec. 3.4). To confirm the reproducibility of the results, we prepared eight homogeneous phantoms on different days and/or at different times and compared their optical properties. The thickness of the upper layer and optical properties of phantoms are listed in Table 1.

3.3 Instrumentation

A single-channel TRS instrument³⁴ (TRS-10, Hamamatsu Photonics KK, Hamamatsu, Japan) was employed in this study. In the TRS-10, three laser diodes with different wave-

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Phantom Name	Optical Coefficient at 760 nm (Prepared Value)/mm ⁻¹				
Homogeneous		μ_a	$\mu_{ m s}'$		
SO	_	0.003	1.0	-	
S1		0.008	1.0		
Two-Layered	Upper Layer			Lower Layer	
	Thickness/mm ⁻¹	μ_{a}	μ_s'	μ_{a}	$\mu_{ m s}'$
LO	10	0.003	1.0	0.003	1.0
LI	10,15	0.013	1.0	0.008	1.0
L2	10,15	0.003	1.0	0.008	1.0
L3	15	0.003	1.0	0.004	1.0
L4	10	0.003	1.0	0.015	1.0
L5	10	0.003	1.0	0.017	1.0
L6	10,15	0.0105	1.0	0.008	1.0
L7	10,15	0.019	1.0	0.015	1.0
L8	10	0.003	1.0	0.008	1.2
L9	10	0.018	1.0	0.020	1.2
L10	10	0.003	1.2	0.004	1.0
L11	10	0.003	1.2	0.008	1.0
L12	10	0.013	1.5	0.008	1.0
L13	10	0.003	1.2	0.008	1.2

Table 1 Sets of optical properties at 760 nm of gelatin phantoms used in experiment, where μ_a and μ'_s are theoretical values based on the concentration of ink and Intralipid, respectively.

lengths (760, 800, and 830 nm) generate optical light pulses having duration of around 100 ps (full width at half maximum; FWHM) at the repetition rate of 5 MHz. After adjusting the intensity by an optical attenuator, light pulses are delivered to the sample through an optical light guide [GI type, 200 μ m core diameter, numerical aperture (NA)=0.25]. The strongest power irradiated to the sample is around 30 μ W at each wavelength. The light pulses passing through the sample are collected by a fiber bundle (3 mm diameter, NA=0.21), and transmitted to a high-speed photomultiplier tube with S-25 photocathode (H6279-MOD, Hamamatsu Photonics KK, Japan) for single-photon detection in the NIR light region. A circuit for time-resolved measurement based on timecorrelated single-photon counting (TCSPC) method measures the temporal profile. Minimal data acquisition time is 100 ms.

3.4 Time-Resolved Measurement and Determination of Optical Properties of Phantoms

In phantom experiments, as shown in Fig. 2, incident and detecting light guide with a separation of 30 mm were placed on the upper surface of a phantom. Measurements with an accumulation time of 10 s were performed at more than three

different positions within an area 40 mm apart from the edge of the phantom to avoid the distortion of photon diffusion due to the edge. The count rate was adjusted to 100 to 150 kcps at each wavelength by optical attenuator to prevent the pile-up distortion. We avoided specular reflection and light leakage by employing a black light-guide holder. In every experiment, the instrumental responses of the TRS-10 were measured, facing the input and receiving fibers each other through a neutral density filter in a black tube. The instrumental response was around 150 ps FWHM at each wavelength.

Optical properties in homogeneous phantoms and in each layer of the two-layered phantoms were determined by fitting an analytical solution of the photon diffusion equation to the measured temporal profile with nonlinear least squares regression. The data in a time range of 0 to 5400 ps were selected for fitting. In obtaining the analytical solution, the extrapolated boundary condition of reflectance mode^{35,36} was employed. The theoretical profile was convoluted with the measured incident pulse shape in the fitting process. Light velocity in gelatin was assumed to be 0.225 mm/ps, corresponding to its refractive index of 1.33. The same values of these were also used for the calculation of μ_a^{seg} .



Fig. 2 Schematic of the measurement for samples. It performed by reflectance mode, in which both light guides for radiation and detection are arranged in parallel. A mat black plate that has holes for light guides is on the samples as a light guide holder to decrease the error due to specular reflection and light leakage.

4 Results

4.1 *Monte Carlo Simulation*

4.1.1 Temporal variations of μ_a^{seg}

First we examined the temporal variations of μ_a^{seg} under several conditions in which the μ_a of each layer were changed. As a matter of convenience, the segments were numbered as I, II, III, etc. in order of time starting from t=500 ps (e.g., the segment by time range from 500 to 1000 ps was denoted as segment I and that from 2500 to 3000 ps was as segment V, and so on). Figure 3 shows the variations of $\mu_a^{\text{seg}}(K)$ (K =segment number) of media, the upper layer thickness of which was 10 mm and μ'_s of both layers were 1 mm⁻¹. The $\mu_a^{\text{seg}}(K)$ are expressed as the ratio to the real $\mu_{a,\text{lower}}$. A homogeneous medium was used as a reference profile (μ'_s =1 mm⁻¹, μ_a =0.005 mm⁻¹). Roughly, three types of the $\mu_a^{\text{seg}}(K)$ curves were observed. The $\mu_a^{\text{seg}}(K)$ in the case of the identical μ_a between the two layers were almost constant in all the time segments. In the case where $\mu_{a,\mathrm{upper}}$ was larger than $\mu_{a,\text{lower}}$, the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$ was above 1 at 0.5 to 1 ns (segment I) and gradually decreased with time, converging on 1 in 2.5 to 3.5 ns (segments V and VI). On the other hand, in the case where $\mu_{a,\text{upper}}$ was smaller than $\mu_{a,\text{lower}}$, $\mu_a^{\text{seg}}(I)$ was below 1 at 0.5 to 2 ns and increased with time. Even in a later time period, $\mu_a^{seg}(K)$ did not reach the $\mu_{a,\text{lower}}$.

4.1.2 Effects of the difference in scattering on μ_a^{seg}

Next, using two additional two-layered models in which upper μ'_s was different from the lower μ'_s , we examined the effects of the difference in μ'_s between the two layers on the $\mu^{\text{seg}}_a(K)$. Figure 4(a) shows the temporal variations of $\mu^{\text{seg}}_a(K)$ of the media with different μ'_s between the two layers as well as those of media with the same μ'_s . As the reference profile, a homogeneous medium in which μ'_s was the same as that of the upper layer ($\mu'_s = 1$ or 1.5 mm⁻¹, $\mu_a = 0$ mm⁻¹) was used.



Fig. 3 Temporal variations of $\mu_a^{\text{seg}}(K)$ of the two-layered media, where the upper layer thickness was 10 mm and μ'_s of both layers were 1 mm⁻¹, predicted by Monte Carlo simulation. The vertical axis represents the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$. A homogeneous medium was used as a reference profile ($\mu'_s = 1 \text{ mm}^{-1}$, $\mu_a = 0.005 \text{ mm}^{-1}$).

The vertical axis represents the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$. Even though upper and lower μ'_s values were different from each other in the range from 1.0 to 1.5 mm⁻¹, the temporal variation of $\mu_a^{\text{seg}}(K)$ was very similar to that in the case in which both layers had the same μ'_s .

Figure 4(b) shows the effects of the μ'_s difference between an object and a reference on the temporal variations of $\mu_a^{\text{seg}}(K)$. Each $\mu_a^{\text{seg}}(K)$ was calculated by a reference in which μ'_s was the same (1.0 mm⁻¹) as, larger (1.2 mm⁻¹) than, and smaller (0.8 mm⁻¹) than that of upper layer of an object. When we used a reference with larger μ'_s , $\mu_a^{\text{seg}}(K)$ in the earlier time segments were larger than μ_a estimated by a reference with the same μ'_s . In contrast, when a reference with smaller μ'_s was used, $\mu_a^{\text{seg}}(I)$ was smaller than that in the case of the same μ'_s . The $\mu_a^{\text{seg}}(I)$ calculated by a 1.2-mm⁻¹ reference and the $\mu_a^{\text{seg}}(V)$ and (VI) by the 0.8-mm⁻¹ reference were almost equal to that calculated by the reference with the same μ'_s (1.0 mm⁻¹).

4.1.3 Effect of the μ_a difference between the upper and lower layer on the μ_a^{seg} in later segments

Figure 5 shows the $\mu_a^{\text{seg}}(\text{IV})$ (V), and (VI) of two-layered media (upper layer thickness=10 mm) predicted by Monte Carlo simulation as a function of the ratio of $\mu_{a,\text{upper}}$ to $\mu_{a,\text{lower}}$ (μ_a ratio_{upper/lower}). The data obtained in the cases in which μ'_s was equal (the models in Sec. 4.1.1) and different (the models in Sec. 4.1.2) between the two layers were plotted together. As the reference profile, a homogeneous medium in which μ'_s was the same as that of the upper layer was used. When the μ_a ratio_{upper/lower} was equal to or more than 1, the $\mu_a^{\text{seg}}(\text{IV})$, (V), and (VI) nearly represented the real μ_a . The error was less than 5.0% in segment VI. On the other hand, the $\mu_a^{\text{seg}}(K)$ even in these later time periods were smaller than the real μ_a in the range of the μ_a ratio_{upper/lower} less than 1. The deviation grew larger as the μ_a ratio_{upper/lower} decreased.



Fig. 4 (a) Temporal variations of $\mu_a^{\text{seg}}(K)$ of two-layered media with different μ'_s between the two layers together with those of media with the same μ'_s predicted by Monte Carlo simulation. The upper layer thickness was 10 mm. As a reference profile, a homogeneous medium in which μ'_s was the same as that of the upper layer ($\mu'_s=1$ or 1.5 mm⁻¹, $\mu_a=0.005$ mm⁻¹) was used. The vertical axis represents the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$. (b) Temporal variations of $\mu_a^{\text{seg}}(K)$ of two-layered media (upper layer: $\mu'_s=1$ mm⁻¹, $\mu_a=0.015$ mm⁻¹, lower layer: $\mu'_s=1$ mm⁻¹, $\mu_a=0.015$ mm⁻¹, provide the same as that of the upper layer thickness of the two-layered media (upper layer: $\mu'_s=1$ mm⁻¹, $\mu_a=0.015$ mm⁻¹, lower layer: $\mu'_s=1$ mm⁻¹, $\mu_a=0.01$ mm⁻¹; upper layer thickness=10 mm) predicted by Monte Carlo simulation and analyzed using three different homogeneous references [$\mu'_s=0.8$ (Δ), 1.0 (\blacksquare), 1.2 mm⁻¹ (\bigcirc); $\mu_a=0.005$ mm⁻¹].

4.2 Phantom Experiment

4.2.1 Optical properties of phantoms

Maximum deviation of the optical properties of phantoms in intra- and inter-samples from the mean value were 3 and 8%, respectively. Temporal profiles of detected light intensity in homogeneous (S0) and two-layered phantom (L0), which consists of two layers with the same optical properties as those of S0, were almost in agreement (data not shown). It was thus concluded that the effect of the interface between two layers on the pattern of photon propagation was negligible in present study conditions.



Fig. 5 The μ_a^{seg} (IV) (\Box), (V) (\blacklozenge), and (VI) (\triangle) of two-layered media predicted by Monte Carlo simulation as a function of the ratio of $\mu_{a,\text{upper}}$ to $\mu_{a,\text{lower}}$ (μ_a ratio_{upper/lower}). Upper layer thickness was 10 mm. The data in both cases that μ'_s was identical or different between the two layers were plotted together. A homogeneous medium in which μ'_s was the same as that of the upper layer was used as the reference profile.

4.2.2 Temporal variation of μ_a^{seg}

Whichever wavelength (760, 800, and 830 nm) we used, the results obtained from the following analyses of phantoms were almost the same. Thus, we present the data at 760 nm as representative results. In the phantoms with values of μ_a larger than 0.015 mm⁻¹, the profiles of $A^{\text{diff}}(t)$ were reliable only in the time range of 0.5 to 2 ns. Therefore, we mainly with results of phantoms show the μ_a of 0.003 to 0.013 mm⁻¹, for which our instrument shows adequate performance, although they were smaller than that of human head generally estimated. Figure 6 shows the typical time-resolved reflectance [Fig. 6(a)] and $A^{\text{diff}} - t$ curve [Fig. 6(b)] obtained by phantom measurements. In this condition, the data were reliable in the time period from 0.35 to 3 ns. In the early time period before 0.25 ns and in the later time period after 3 ns, data were noisy because of the interaction of incident light and/or the decrease in detected photon numbers. Therefore, analysis for slope of $A^{\text{diff}}(t)$ (calculation of μ_a^{seg}) was performed in the range of 0.5 to 3 ns. The segments were numbered as I, II, III, etc. in order of time in the same manner as the case in Sec. 4.1.

Figure 7 shows temporal variations of $\mu_{a}^{seg}(K)$ in twolayered phantoms (measured optical properties of L1: μ'_s = 1.14±0.02 mm⁻¹, $\mu_{a,upper}$ =0.0143±0.0001 mm⁻¹, $\mu_{a,lower}$ =0.0088±0.0002 mm⁻¹; L2: μ'_s =1.12±0.01 mm⁻¹, $\mu_{a,upper}$ =0.0030±0.0001 mm⁻¹, $\mu_{a,lower}$ =0.0081±0.0001 mm⁻¹) with the upper layer thickness of 10 mm as well as that of the homogeneous phantom (S1: μ'_s =1.06±0.02 mm⁻¹, μ_a =0.0084±0.0002 mm⁻¹). The $\mu_a^{seg}(K)$ are expressed as the ratio to the real $\mu_{a,lower}$. The μ'_s of the reference was the same as that of the upper and lower layers of these phantoms. The $\mu_a^{seg}(K)$ of S1 were almost constant in all the time segments, and the ratio to the real $\mu_{a,lower}$ was 0.96±0.06. As for L1 (μ_a ratio_{upper/lower}=1.66), the ratio of $\mu_a^{seg}(I)$ to the real $\mu_{a,lower}$ was 1.37±0.05. It



Fig. 6 Typical time-resolved reflectance and $A^{\text{diff}} - t$ curve obtained by phantom measurements: (a) temporal profiles of incident light (IN), intensity of the detected light through a homogeneous $[I_R(t)]$ and a two-layered medium [I(t)] and (b) $A^{\text{diff}} - t$ curve obtained from the data in (a) in the time period of 0 to 4 ns. The data of detected light intensity through the phantoms are deconvoluted by the temporal profile of the incident light and A^{diff} at each time was calculated. The Roman numerals show numbers of segments of the curve parted every 0.5 ns to get the μ_a^{seg} .

gradually decreased with time to 0.98 ± 0.07 in segment IV and 0.91 ± 0.01 in segment V. On the other hand, in L2 $(\mu_a \text{ratio}_{upper/lower}=0.40)$, $\mu_a^{seg}(I)$ was 0.56 ± 0.04 and increased with time to 0.80 ± 0.05 in ~ 3 ns (segment V).

Figure 8 shows the temporal variations of $\mu_a^{\text{seg}}(K)$ of phantoms with an upper layer thickness of 15 mm. The optical properties of each layer in L1' and L2' were the same as those of L1 and L2, respectively. For comparison, $\mu_a^{\text{seg}}(K)$ of S1 is also shown. Like in the phantoms with an upper layer thickness of 10 mm shown in Fig. 7, the pattern of $\mu_a^{\text{seg}}(K)$ was dependent on $\mu_{a,\text{upper}}$. When $\mu_{a,\text{upper}}$ was larger than $\mu_{a,\text{lower}}(\text{L1'})$, the $\mu_a^{\text{seg}}(\text{V})$ indicated $\mu_{a,\text{lower}}$.

The effects of the scattering difference on the temporal variations of $\mu_a^{\text{seg}}(K)$ were found in a similar manner to the results by Monte Carlo simulation (data not shown).

4.2.3 Effect of the μ_a difference between the upper and lower layer on the μ_a^{seg} in later segments

Figure 9 shows the μ_a^{seg} in segment IV [Fig. 9(a)] and segment V [Fig. 9(b)] as a function of μ_a ratio_{upper/lower} by mea-



Fig. 7 Temporal variations of $\mu_a^{\text{seg}}(K)$ of two-layered phantoms (L1 and L2), of which upper layer thickness was 10 mm, and homogeneous phantom of S1 (L1: $\mu'_s = 1.14 \pm 0.02 \text{ mm}^{-1}$, $\mu_{a,upper} = 0.0143 \pm 0.0001 \text{ mm}^{-1}$, $\mu_{a,lower} = 0.0088 \pm 0.0002 \text{ mm}^{-1}$; L2: μ'_s $\mu_{a,\text{upper}} = 0.0030 \pm 0.0001 \text{ mm}^{-1}$, $=1.12\pm0.01$ mm⁻¹, $\mu_{a,\text{lower}}$ $= 0.0081 \pm 0.0001 \text{ mm}^{-1};$ $\mu_s' = 1.06 \pm 0.05 \text{ mm}^{-1}$ S1: μ_a =0.0084±0.0002 mm⁻¹). A homogeneous phantom S0 (μ'_s =1.01±0.04 mm⁻¹, μ_a =0.0030±0.0001 mm⁻¹) was used as a reference. The plots represent mean ±SD (standard deviation) ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$ (L1, L2: n=3 positions $\times 2$ samples; S1: n= 3 positions \times 8 samples). Top dotted line and bottom broken line indicate the real $\mu_{a,\text{upper}}$ shown as the ratio to the real $\mu_{a,\text{lower}}$ in L1 and L2, respectively.

surements of phantoms in Table 1. As in the Monte Carlo simulation, the $\mu_a^{\text{seg}}(K)$ in later time periods depended on the difference in μ_a values between the upper and the lower layers: it was smaller than the real $\mu_{a,\text{lower}}$ in the range of the μ_a ratio_{upper/lower} less than 1, while it almost represented the real $\mu_{a,\text{lower}}$ when the μ_a ratio_{upper/lower} was equal to or more than 1. In the case in which upper layer thickness was 15 mm, the μ_a^{seg} was much smaller in the range of the μ_a ratio_{upper/lower} was equal to or more than 1.



Fig. 8 Temporal variations of $\mu_a^{\text{seg}}(K)$ of two-layered phantoms (L1' and L2'), of which the upper layer thickness was 15 mm, and homogeneous phantom of S1 at 760 nm using S0 (μ'_s =1.0 mm⁻¹, μ_a =0.003 mm⁻¹) as a reference. The optical properties of each layer in L1' and L2' are the same as L1 and L2. The notation of the vertical axis is the same as that of Fig. 7. Values are means ±SD (L1', L2': n=3 positions ×2 samples, S1: n=3 positions ×8 samples). Top dotted line and bottom broken line represent the real $\mu_{a,\text{upper}}$ shown as the ratio to the real $\mu_{a,\text{lower}}$ in L1' and L2', respectively.



Fig. 9 Plots of μ_a^{seg} in (a) segment IV and (b) segment V in reference to the ratio of $\mu_{a,\text{upper}}$ to $\mu_{a,\text{lower}}$ ($\mu_a\text{ratio}_{\text{upper/lower}}$) of three kinds of phantoms (Table 1); upper layer thickness is 10 mm and μ'_s of both layers are the same as the reference (\blacksquare), upper layer thickness is 10 mm and μ'_s of the lower layer is different from the reference (\square), and upper layer thickness is 15 mm and μ'_s of both layers are the same as the reference (\blacksquare). The vertical axis represents the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$. Each plot was average value by several measurements for one sample.

below 1, while it was larger than the real values in the range of the μ_a ratio_{upper/lower} above 1 in segment IV, but not in segment V. When the μ'_s value of the lower layer was different from that of the reference, there were no significant changes in the relationship between the μ_a ratio_{upper/lower} and the $\mu_a^{seg}(IV)$ or (V).

5 Discussion

5.1 Relationship Between μ_a^{seg} and Real μ_a of Each Layer

Time segment analysis, dividing the temporal profile of detected light intensity into segments, leads to some findings on path distribution in the direction of depth of photons detected at each time for layered turbid media with absorbers.

The results obtained from the analyses for Monte Carlo simulation data were generally confirmed by those of phantom experiments data. As one of the mutual results, it was found that the μ_a^{seg} values in later segments depended on the difference in real μ_a between two layers. This represents that in later time, the partial path length in each layer depends on both μ_a values of the layers because the probability that the photons mainly passed in the larger μ_a layer are detected declines. When $\mu_{a,\text{upper}}$ is smaller than $\mu_{a,\text{lower}}$, $l_{\text{upper}}/l_{\text{lower}}$ at a later time is relatively high and $\Delta l_{\rm upper}$ cannot be ignored even in later time segments. Thus, μ_a^{seg} was underestimated by the effect of $\mu_{a,upper}$. In contrast, when $\mu_{a,upper}$ is equal to or larger than $\mu_{a,\text{lower}}$, l_{lower} of photons detected later in time is sufficiently longer than l_{upper} and steadily increase with t, that is, $(\Delta l_{upper}/\Delta L)$ can be considered nearly zero in later time periods, as expected. The presented results, for which μ_a^{seg} were underestimated if $\mu_{a,\text{upper}}$ was smaller than $\mu_{a,\text{lower}}$, were in agreement with a study by Hielscher et al.,²² who employed a curve-fitting method with homogeneous diffusion equation to later part of the time-resolved reflectance.

Similarly, $\mu_a^{\text{seg}}(I)$ did not give the real $\mu_{a,\text{upper}}$ values correctly, which were also affected by the difference in μ_a between two layers (data not shown). As shown in Fig. 1, the photons detected at 500 to 1000 ps have a low probability of

passing through layers lower than the depth of 10 mm. Although Δl_{upper} is dominant to ΔL , $\Delta l_{lower}/\Delta L$ cannot be taken as zero even in this period, especially when the thickness of the upper layer is less than 10 mm. To estimate $\mu_{a,upper}$ more properly, it might be effective to use an earlier time segment of $A^{diff}-t$ curve (e.g., at 350 to 700 ps). But due to the interference of incident light, it seems difficult to select the optimal time period in practical measurements.

5.2 Estimation of μ_a ratio_{upper/lower} by the Ratio of μ_a^{seg} at an Early Time to that at a Later Time

In spite of the discrepancy of μ_a^{seg} from the real μ_a , our method gives us enough information to know the difference in μ_a between the upper and lower layers. Moreover, based on the relationship between the extent of underestimation of μ_a and the ratio of the real μ_a of two layers (Fig. 5), we would derive $\mu_{a,\text{lower}}$ by correction of μ_a^{seg} under the condition where μ'_s of the upper layer and that of a reference are the same and upper layer thickness is almost known. For judgment of the μ_a ratio_{upper/lower}, we attempted to use the μ_a^{seg} at an early time (segment I) and at a later time (segment V) (μ_a^{seg} ratio_{I/V}). First, under the condition where μ'_s of the reference was the same as that of the upper layer of the medium, we examined μ_a^{seg} ratio_{I/V} of various media with different the μ_a ratio_{upper/lower} predicted by the Monte Carlo simulation. Figure 10 shows the plots of $\mu_a \text{ratio}_{\text{upper/lower}}$ to $\mu_a^{\text{seg}} \text{ratio}_{\text{I/V}}$. There was a strong linear correlation between these values $(r^2=0.99)$. Then we checked the relationship between the ratio of the μ_a^{seg} (V) to the real $\mu_{a,\text{lower}}$ and the μ_a^{seg} ratio_{I/V} for both data sets by Monte Carlo simulation [Fig. 11(a)] and by phantom experiment [Fig. 11(b)]. In the range of this ratio below 1, the $\mu_a^{\text{seg}}(V)/\mu_{a,\text{lower}}$ linearly related to the μ_a^{seg} ratio_{I/V}, i.e., we could express them as $\mu_a^{\text{seg}}(V)/\mu_{a,\text{lower}}$ $=a \times \mu_a^{\text{seg}} \text{ratio}_{I/V} + b$, where a and b are constants. By regression analysis, the relationships and the correlation coefficients were a=0.85, b=0.16, and r=0.80 in the plot with Monte Carlo data, and a=0.84, b=0.18, and r=0.96 in that by the phantom experiment, which were almost in agreement. Seg-



Fig. 10 Plots of the ratio of $\mu_{a,\text{upper}}$ to $\mu_{a,\text{lower}}$ (μ_a ratio_{upper/lower}) in reference to the ratio of $\mu_a^{\text{seg}}(I)$ to (V) (μ_a^{seg} ratio_{I/V}) for the Monte Carlo simulation data.

ment IV and segment VI could also be used for the estimation of $\mu_{a,\text{lower}}$. But under the condition of this study, segment V was the most adequate to analyze $\mu_{a,\text{lower}}$, because segment IV included more information of the upper layer [cf. the case of the upper thickness of 15 mm in Fig. 9(a)] and segment VI had higher noise than segment V.

Consequently, we could evaluate $\mu_a \operatorname{ratio}_{upper/lower}$ from $\mu_a^{\operatorname{seg}} \operatorname{ratio}_{I/V}$ and we could estimate the $\mu_{a, \operatorname{lower}}$ by dividing $\mu_a^{\operatorname{seg}}(K)$ in later time by the value of $(a \times \mu_a^{\operatorname{seg}} \operatorname{ratio}_{I/V} + b)$. In Fig. 11, the data in both cases in which μ'_s was equal and different between the two layers within the range of 1.0 to 1.5 mm⁻¹ were plotted together. Therefore, the equation for the relation between $\mu_a^{\operatorname{seg}}(V)/\mu_{a, \operatorname{lower}}$ and $\mu_a^{\operatorname{seg}} \operatorname{ratio}_{I/V}$ holds its validity at least under the condition that μ'_s is 1.0 to 1.5 mm⁻¹ and μ_a is 0.003 to 0.02 mm⁻¹ of each layer in the two-layered media.

5.3 Effect of the Scattering Coefficient on Estimation of μ_a of the Lower Layer

As shown in Fig. 4(a), although the μ'_s of the lower layer was different from that of the reference, the μ^{seg}_a values were almost identical with those for the case where the μ'_s of the

lower layer was the same as that of the reference. In contrast, as shown in Fig. 4(b), the difference in μ'_s between the upper layer and the reference significantly influenced the μ_a^{seg} in earlier time segments. These results indicate that $S^{\text{diff}}(t)$ in Eq. (2) is almost equal to the difference in scattering function only between the shallower part of the media and the reference. In addition, our results showed that the dependence of μ_a^{seg} after 2.5 ns on the difference in μ'_s between the upper layer and the reference was weak. These results are explained by the analytical solution derived by Patterson et al. [Eqs. (7) and (8), Ref. 18]. In the case of homogeneous media, time differential of $S^{\text{diff}}(t)$ in Eq. (2) [or in the first line of Eq. (3)] in this paper can be represented as follows: $dS^{\text{diff}}(t)/dt = [\rho^2/(4D_Rc_R)]$ $-\rho^2/(4D_0c)]/t^2$, where D_R and D_O are the diffusion coefficients for the reference and the object, respectively. As $\left[\rho^2/(4D_Rc_R) - \rho^2/(4D_Oc)\right]$ is constant, $dS^{\text{diff}}(t)/dt$ is in proportion to the reciprocal of the square of time. Thus, the $dS^{diff}(t)/dt$ is negligible at the later time. Similarly, in the case of the two-layered media, it can be considered that $dS^{diff}(t)/dt$ is very small at the later time, i.e., the effect of the μ'_s difference on the μ^{seg}_a at the later time segments can be negligible. In contrast, the scattering term cannot be ignored in the segment I.

5.4 Determination of Proper Reference with Time Segment Analysis

We have showed so far the results mainly in the case where μ'_s of the reference was the same as that of the upper layer of the medium. However, for proper analysis with the correction in Sec. 5.2, we must select an adequate reference with μ'_s very close to that of the upper layer of the target medium that was actually unknown. We can show one of the methods to determine the adequate reference.

As for a homogeneous medium, if μ'_s of an object and a reference are the same, which implies $S^{\text{diff}}(t)$ is zero in Eq. (2), the $A^{\text{diff}}-t$ relation becomes linear. That is, if we select a reference that makes $A^{\text{diff}}(t)$ a straight line, the μ'_s of the reference is the same as that of the object.³⁷ In layered media, as mentioned in Sec. 5.3, $S^{\text{diff}}(t)$ mainly depended on the difference in μ'_s between the upper layer and the reference.



Fig. 11 Plots of μ_a^{seg} (V) with reference to the ratio of the μ_a^{seg} (I) to (V) ($\mu_a^{\text{seg}} \text{ratio}_{|V|}$) in (a) Monte Carlo simulation data and (b) two-layered phantoms with an upper layer thickness of 10 mm (\Box) and 15 mm (\bullet), analyzed by a reference of which μ_s' was the same as that of the upper layer. The vertical axis represents the ratio of $\mu_a^{\text{seg}}(K)$ to the real $\mu_{a,\text{lower}}$. Broken lines are regression lines within the range of $\mu_a^{\text{seg}} \text{ratio}_{|V|}$ below 1.



Fig. 12 (a) The $A^{\text{diff}}-t$ curves of a two-layered medium (upper layer: $\mu'_s = 1 \text{ mm}^{-1}$, $\mu_a = 0.01 \text{ mm}^{-1}$; and lower layer: $\mu'_s = 1.5 \text{ mm}^{-1}$, $\mu_a = 0.015 \text{ mm}^{-1}$; upper layer thickness = 10 mm) in 400 to 1000 ps, predicted by Monte Carlo simulation and analyzed using five references that had various μ'_s values within the range of 0.6 to 1.4 mm^{-1} ($\mu_a = 0 \text{ mm}^{-1}$). (b) Estimated value of $\mu_{a,\text{lower}}$ and the error caused by analyzing with each reference which μ'_s was within the range of 0.8 to 1.6 mm^{-1}. The correction of μ^{seg}_a (V) with the equation in Sec. 5.2 was used to estimate these μ_a values.

Thus, we applied the precedings concept that $S^{\text{diff}}(t)$ is estimated based on the degree of linear relation for $A^{diff} - t$ curve to two-layered media to select an adequate reference. Figure 12(a) shows $A^{\text{diff}} - t$ curves of two-layered medium (upper layer, $\mu'_s = 1 \text{ mm}^{-1}$, $\mu_a = 0.01 \text{ mm}^{-1}$, and lower layer, μ'_s =1.5 mm⁻¹, μ_a =0.015 mm⁻¹, upper layer thickness =10 mm) in 400 to 1000 ps, predicted by Monte Carlo simulation and analyzed using five references that had different μ'_s values within the range of 0.6 to 1.4 mm⁻¹ ($\mu_a = 0$ mm⁻¹). We examined the coefficient of determination r^2 of each curve by linear regression analysis. It could be found that when a reference was used whose μ'_s was the same as that of the upper layer of an object, r^2 was extremely close to 1. It indicates that when thickness of the upper layer is larger than 10 mm, the change in $\mu_a^{\text{diff}}(t)$ with t is so small as compared with that of $S^{\text{diff}}(t)$ in time segment I and in time earlier than segment I. Thus, using this method of investigating linear relation for $A^{\text{diff}} - t$ at an earlier time, we can select an appropriate reference. Figure 12(b) shows estimated μ_a values of the lower layer and the errors for this model analyzed by various references already described. The correction of μ_a^{seg} (V) with equation in Sec. 5.2 was used to estimate these μ_a . It was found that when a reference was used whose μ'_s value was the same as that of the upper layer of an object, the estimated μ_a was almost the same as the real μ_a . We also found that when the difference in μ'_s between a reference and the upper layer of an object was smaller than 0.5 mm⁻¹, the error of estimated μ_a was less than 10%. In other words, we should prepare a series of reference in which μ'_s were changed by every 0.5 mm⁻¹ within the range of the human extracerebral tissue to estimate reliable μ_a by this method.

5.5 Possibility of Applying the Present Method to Human Head Measurements

The time segment analysis of time-resolved reflectance in two-layered media enabled us to simply acquire information on the μ_a of each layer and was implemented for a reflectance by measurement with a single source-detector distance. Moreover, we found that the estimated value of $\mu_{a,\text{lower}}$ depended on the value of μ_a ratio_{upper/lower}, i.e., μ_a^{seg} were underestimated if $\mu_{a,\text{upper}}$ was smaller than $\mu_{a,\text{lower}}$, which was almost the same as the results in the case of fitting analysis for the later part of time-resolved reflectance by a solution of diffusion equations for homogeneous media.²² In our method, however, the difference in μ_a (μ_a ratio_{upper/lower}) can be evaluated using μ_a^{seg} both at earlier time and at later time (μ_a^{seg} ratio_{I/V}).

For the adult human forehead, the total thickness of scalp and skull is^{28,38} about 10 mm. Thus, the μ_a of the brain may be estimated by μ_a^{seg} (IV) to (VI) if the human head could be approximated to two-layered model. On the other hand, the human head is a multilayered structure and the scattering phenomenon must be more complex. Therefore we require further experiments with a more sophisticated model of the human head to confirm the utility and limitations of this method. For example, relation between the discrepancies of estimated μ_a from the real μ_a and the ratio of μ_a^{seg} at an earlier time to that at a later time in multilayered models, and dependence of the layer thickness on the relationship should be examined. As the segment size, a time range of 500 ps was chosen in this study. For a multilayered model, however, we should evaluate the segment size to obtain better results. Moreover reliable estimation requires determining μ'_s values of the scalp and skull, which vary with individuals and each position on the head.

6 Conclusion

We confirmed that the "time segment analysis" of time resolved reflectance for a two-layered media could selectively determine the values of $\mu_{a,\text{lower}}$. Under the condition where μ'_s of a reference profile is the same as that of the upper layer of an object medium, this analysis enables us to estimate the deference in μ_a between the upper and the lower layers. It was also possible to determine $\mu_{a,\text{lower}}$ by correcting the μ_a^{seg} with the ratio of μ_a^{seg} in an earlier time segment and to that in a later one if we have rough knowledge of the upper layer thickness. In conclusion, the presented approach has a potential to selectively determine the value of μ_a and to quantitatively evaluate concentrations of the Hb in human cerebral tissue.

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