Measurement of oxygen saturation in small retinal vessels with adaptive optics confocal scanning laser ophthalmoscope

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Abstract. We have used an adaptive optics confocal scanning laser ophthalmoscope to assess oxygen saturation in small retinal vessels. Images of the vessels with a diameter smaller than 50 μm are recorded at oxygen sensitive and isosbestic wavelengths (680 and 796 nm, respectively). The vessel optical densities (ODs) are determined by a computer algorithm. Then, OD ratios (ODRs), which are inversely proportional to oxygen saturation, are calculated. The results show that arterial ODRs are significantly smaller than venous ODRs, indicating that oxygen saturation in the artery is higher than that in the vein. To the best of our knowledge, this is the first noninvasive measurement of oxygen saturation in small retinal vessels.

Keywords: adaptive optics confocal scanning laser ophthalmoscope; retinal oximetry; retinal image registration; spectrophotometry.

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The retina has a high demand for oxygen, and retinal hypoxia is believed to be an important factor in retinal diseases, such as diabetic retinopathy, glaucoma, and arteriogenous occlusion. Because retinal microvasculature plays an important role in the oxygen supply, the measurement of the oxygen saturation in small retinal vessels would be very useful to diagnose and monitor these diseases.

A lot of noninvasive techniques have been developed to measure the oxygen saturation of retina. Hickham et al. were the first to noninvasively measure the retinal oxygenation using photographic methods. Delori developed a three-wavelength oximetry to obtain oxygen saturation in retinal vessels. Beach et al. presented a digital imaging system to measure oxygen saturation in retinal vessels by dual-wavelength imaging. Khoobehi et al. developed a hyperspectral imaging technique for spatially mapping the relative oxygen saturation in the optic nerve head. Narasimha-Iyer et al. developed automatic algorithms for oximetry with dual-wavelength fundus images. Ramella-Roman et al. introduced a multiaperture camera system for oxygen saturation measurement in retinal vessels.

Kagemann et al. used Fourier domain optical coherence tomography to assess retinal oxygen saturation, and a difference between arterial and venous oxygen saturation was detected. Smith et al. used a scanning laser ophthalmoscope to measure retinal oxygen saturation in vessels with a diameter larger than 50 μm.

However, the image resolution of the above mentioned methods is restricted by ocular aberrations. For the vessels smaller than 50 μm, the image difference between different wavelengths and the vessel profile are difficult to be detected. Thus, it is very difficult to measure oxygen saturation in the vessels smaller than 50 μm, though the small vessels can be imaged. On the other hand, the ocular aberrations can be compensated with adaptive optics (AO) to achieve a nearly diffraction-limited resolution. AO has been combined with adaptive optics (AO) to improve the imaging resolution.

In this study, oxygen saturation in small retinal vessels with diameters ranging from 27 to 49 μm is assessed by AOLO. High resolution retinal vessel images are obtained at oxygen sensitive and isosbestic wavelength (680 and 796 nm, respectively). Optical densities (ODs) of vascular segments are determined by a computer algorithm. Then, the OD ratios (ODRs) that are inversely proportional to the oxygen saturation are calculated.

A dual-wavelength AOSLO system for real-time (30 Hz) retina imaging is used in the experiment. Figure 1 shows a schematic diagram of the setup. A band-filtered beam (680 or 796 nm, 7 nm bandwidth) of light emitted from a superluminescent diode (SLD1: Superlumdiodes Ltd., SLD-261-HP or SLD2: Superlumdiodes Ltd., SLD-381-HP1) is focused to a small spot on the retina. Two scanning mirrors [horizontal scanner (HS): 16 KHz resonant scanner, Electro-Optical Products Corp. vertical scanner (VS): 30 Hz galvometric scanner, Cambridge 6800-HP-3YS] are used to control the focused spot to scan the retina. Light scattered back from the retina is split into two beams. One beam enters a photomultiplier tube (PMT, Hamamatsu H7422-20) for signal detection. By synchronizing the PMT signal and two scanning mirrors, the retinal images can be consecutively recorded. The other beam is captured by a Shack–Hartmann wavefront sensor (WS) with 97 effective sub-apertures in 11×11 arrays. The slope data of the wavefront are acquired by a computer and transferred to control signals for a 37-channel deformable mirror (DM). After 20 to 30 iterations, the error of the corrected wavefront approaches the minimum.

The resolution of our imaging system is approximately 2.5 μm laterally and better than 100 μm axial.

Eight normal healthy volunteers (3 female, 5 male, ages range from 22 to 30 years) were recruited for this study. To control the image location, a computer-controlled 8×8 LED array fixation target was provided for the volunteer to view while imaging. In order to find the best imaging plane of blood vessels, defocus was applied to section the retina axially. Video clips of retinal vessels at 680 and 796 nm were recorded sequentially. The frame size is 512×480 pixels, and the field of view is 1.5 deg. The time interval between two wavelengths switching is approximately 3 s. Four sequential frames were averaged to improve the image quality.
Fig. 1 Schematic of a dual-wavelength AOSLO system. HS, horizontal scanner; VS, vertical scanner; WS, wavefront sensor; DM, deformable mirror; PMT, photomultiplier tube; BS1, BS2, BS3, beam splitters; BF1, BF2, band filters; CL, collecting lens; FM1, FM2, folding mirrors; SLD1, SLD2, superluminescent diodes; M1 ∼ M8, spherical mirrors; PH, pinhole; TL, trial lens.

Due to the eye motion, the retinal images at different wavelengths have to be registered. The similarity between the images at 680 and 796 nm is determined using mutual information,

$$I(A, B) = \sum_{i,j} p_{AB}(i, j) \log \left( \frac{p_{AB}(i, j)}{p_A(i, j) \cdot p_B(i, j)} \right), \quad (1)$$

where $p_{AB}(i, j)$ is the joint probability distribution of images $A$ and $B$, and $p_A(i, j)$ and $p_B(i, j)$ are probability distributions of images $A$ and $B$, respectively. $p_{AB}(i, j)$ can be estimated by calculating a normalized joint histogram of the gray values, and $p_A(i, j)$ and $p_B(i, j)$ can be estimated by calculating a normalized histogram. The image at 680 nm was used as a reference. A subimage from the image at 796 nm was translated and rotated to maximize $I(A, B)$ of the subimage and the reference image. Then, the translation and the rotation of the image at 796 nm were determined, and the images were registered.

After the registration, a computer program was used to obtain the paths by tracking the minimum intensity inside the vessel and the outside intensity at a fixed distance from the minimum intensity. The paths were identified in the 796 nm images, and the corresponding paths on the 680 nm images were also determined. The results are shown in Table 1. As is shown in Table 1, vascular ODR in Fig. 2(a) is significantly smaller than that in Fig. 2(c). This suggests that the vascular oxygen saturation in Fig. 2(a) is higher than that in Fig. 2(c).

A fundus camera (Cannon CR6-45NM) was used to identify retinal arteries and veins. A fundus camera image is shown in Fig. 3, and the field of view is 37 deg. The black and white rectangles in Fig. 3 represent the regions in Figs. 2(a) and 2(c), respectively. Arteries and veins were identified by visual inspection of the fundus camera image. The vessel in Fig. 2(a) is an

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<th>Figures</th>
<th>OD_{680}</th>
<th>OD_{796}</th>
<th>ODR</th>
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<tr>
<td>2(a)</td>
<td>0.27</td>
<td>0.49</td>
<td>0.55</td>
</tr>
<tr>
<td>2(c)</td>
<td>0.46</td>
<td>0.48</td>
<td>0.96</td>
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artery and the vessel in Fig. 2(c) is a vein. Thus, the vascular oxygen saturation in Fig. 2(a) is higher than that in Fig. 2(c). This agrees with the results obtained with AOSLO.

ODRs of the eight volunteers’ vessels are presented in Table 2 and the results show that the arterial ODRs are significantly smaller than the venous ODRs (0.60 ± 0.11 and 0.98 ± 0.07, respectively; \( p < 0.00001 \)) (mean ± standard deviation). A significant difference between arterial and venous oxygen saturation is therefore detected.

In summary, AOSLO has been used to assess retinal oxygen saturation. The retinal vessels with diameter ranging from 27 to 49 μm were imaged at two wavelengths (680 and 796 nm), and the ODRs of the vessels between 796 and 680 nm were calculated. The results showed that arterial ODRs were significantly smaller than venous ODRs, indicating that oxygen saturation in the artery is higher than that in the vein. As the oxygen saturation in small vessels can be affected by the metabolic activity in the local areas of the retina, the measurement of the oxygen saturation would be very useful to achieve early assessments of retinal disease associated with oxygen utilization.

### Acknowledgments

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### References


![Fig. 3 A fundus camera image showing the same regions imaged in Fig. 2.](image)